

## Article

# Gold Nanobeads with Enhanced Absorbance for Improved Sensitivity in Competitive Lateral Flow Immunoassays

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**Abstract:** Background: Colloidal gold based lateral flow immunoassay (LFIA) commonly suffers from relatively low detection sensitivity due to the insufficient brightness of conventional gold nanoparticles (AuNPs) with the size of 20–40 nm. Methods: Herein, three kinds of gold nanobeads (GNBs) with the size of 94 nm, 129 nm, and 237 nm, were synthesized by encapsulating numerous hydrophobic AuNPs (10 nm) into polymer matrix. The synthesized GNBs exhibited the enhanced colorimetric signal intensity compared with 20–40 nm AuNPs. The effects of the size of GNBs on the sensitivity of LFIA with competitive format were assessed. Results: The results showed that the LFIA using 129 nm GNBs as amplified signal probes exhibits the best sensitivity for fumonisin B<sub>1</sub> (FB<sub>1</sub>) detection with a cut-off limit (for visual qualitative detection) at 125 ng/mL, a half maximal inhibitory concentration at 11.27 ng/mL, and a detection limit at 1.76 ng/mL for detection of real corn samples, which are 8-, 3.82-, and 2.89-fold better than those of conventional AuNP<sub>40</sub>-based LFIA, respectively. The developed GNB-LFIA exhibited negligible cross-reactions with other common mycotoxins. In addition, the accuracy, precision, reliability, and practicability were demonstrated by determining real corn samples. Conclusions: All in all, the proposed study provides a promising strategy to enhance the sensitivity of competitive LFIA via using the GNBs as amplified signal probes.

**Keywords:** gold nanobeads; lateral flow immunoassay; enhanced sensitivity; mycotoxin; corn sample

## 1. Introduction

Colloidal gold based lateral flow immunoassay (LFIA) is one of the most popular screening tools for on-site bio-detection by the naked-eye because of its advantages, such as simplicity, convenience, rapidity, and low cost [1,2]. For the conventional LFIA, the presence of a red band in the detection line depends on the sufficient gold nanoparticle (AuNP) accumulation [3]. In competitive format, an evident red band at the test line is required when target analytes are absent in the sample solution. Thus, the presence of sufficient AuNPs on the test line is the premise to produce a distinct red band. The color intensity of accumulated AuNPs is associated with the accumulation number and the original color intensity of AuNPs [4]. However, conventional 20–40 nm AuNPs suffer from relatively weak color intensity, thus indicating the need for their increasing accumulation to generate an apparent red band in the test zone [5]. However, an increased AuNP number is non-conductive to the competition inhibition of target analytes and thus leads to decreased sensitivity. Theoretically, improving the color intensity of individual probes can effectively reduce the required number of accumulated probes in the test area for enhanced sensitivity in competitive LFIA. For this purpose, various new nanomaterials with enhanced signal

transducer features, such as quantum dots (QDs) [6], upconversion nanoparticles [7], dye-doped nanoparticles [8], and magnetic nanobeads [9], have been recently introduced to replace AuNPs as LFIA labels to improve the sensitivity. Nonetheless, external excitation and advanced reading devices are necessary for signal acquisition, thereby partially limiting the potential of such nanomaterials in field detection. Thus, the simultaneous enhancement of color signal intensity and the naked-eye-based visual detection capability of conventional AuNP-based colorimetric probes remains a huge challenge.

Nanocontainers are versatile structures containing a considerable number of cavities, holes, or pores that can be applied for loading various materials, such as drugs, enzymes, nanoparticles, and signal-generating molecules [10–12]. At present, the available nanocontainers mainly involve liposomes [13], mesoporous silica [12], proteinsomes [14], and polymer- [15], metal oxide- [16], and carbon-based nanomaterials [17]. The large surface areas and inner volumes of such nanocontainers endow them with superior loading capacity to entrap diverse molecules for wide-ranging applications in drug delivery, bioimaging, bioreactors, and biodetection [18–22]. Polymer nanocontainers, such as polymersomes or polymeric nanocapsules, have attracted increasing interest in the signal amplification systems due to their excellent water solubility, biocompatibility, and colloid stability [23]. On the other hand, polymer nanocontainers are readily synthesized using various methods, including self-assembly-based strategies [24], film hydration methods [25], phase-separation techniques [26], and template polymerization approaches [27,28]. For example, our previous studies reported polymer-based nanocontainers for the encapsulation of highly luminescent CdSe/ZnS QDs by using the self-assembly method [29]. Numerous isolated QDs were tightly embedded in the polymeric nanocapsules. The obtained QD-encapsulated nanocontainers revealed 2863-fold higher luminescent intensity than the original individual QDs. We demonstrated the feasibility of using these QD nanocontainers as enhanced signal reporters in conventional competitive LFIA to improve sensitivity owing to their ultrahigh luminescent signal.

On this basis, herein, we first fabricated a polymer-based nanocontainer for the encapsulation of small size AuNPs to prepare large size gold nanobeads (GNBs) with significantly enhanced absorbance [30]. We also demonstrated the potential of GNBs as amplified labeling probes in competitive LFIA for increased sensitivity. The GNBs were synthesized by encapsulating numerous isolated hydrophobic AuNPs (10 nm) into a polymer matrix of poly(maleicanhydride-alt-1-octadecene) (PMAO) by using the emulsion-based self-assembly strategy. The PMAO matrix was selected as a polymer layer because it can increase the interparticle gap for decreased plasmonic coupling and provide the carboxyl surface for subsequent biomolecule functionalization. Further characterization indicated that the resultant GNBs exhibited a uniform regular sphere with numerous AuNPs internally distributed. The number of embedded AuNPs and the absorbance were tuned by changing the GNB size, providing an opportunity to better investigate the relationship between the GNB size and the analytical performance of LFIA because the GNB size can affect the LFIA sensitivity by influencing the signal intensity and the immunological reaction efficiency [31].

Contamination of cereals and related products by mycotoxins has become an increasingly serious food safety problem. As a common mycotoxin, fumonisins (FBs) are nephrotoxic, hepatotoxic, and carcinogenic mycotoxins mainly produced by *Fusarium* mold species. Among all known FBs, FB<sub>1</sub> almost constitutes about 70% found in contaminated foods. Given its high threat to human and animal health, FB<sub>1</sub> has been regarded as a human group 2B carcinogen by the International Agency for Research on Cancer [32–35]. Hence, the rapid and sensitive detection of FB<sub>1</sub> for food industry is critical to minimize its hazards. Under the optimal condition, the GNBs with size of 129 nm (GNB<sub>129</sub>) as the signal reporter of LFIA featured a high sensitivity in detecting FB<sub>1</sub>. The cut-off limit (for visual qualitative detection), half maximum inhibitory concentration, and detection limit (for quantitative analysis) of GNB<sub>129</sub>-LFIA were 125 ng/mL, 11.27, and 1.76 ng/mL, which were 8-, 3.82-, and 2.89-fold lower than conventional LFIA strip with 40 nm AuNPs (AuNP<sub>40</sub>) as

labeling probes. The specificity, accuracy, reproducibility, reliability, and practicability of our proposed GNB<sub>129</sub>-LFIA were demonstrated in real corn samples. In conclusion, the designed GNBs can act as a promising signal reporter in LFIA to provide an amplified competitive detection for various small molecular chemicals, such as mycotoxins.

## 2. Materials and Methods

### 2.1. Materials and Reagents

Aflatoxin B<sub>1</sub> (AFB<sub>1</sub>), aflatoxin B<sub>2</sub> (AFB<sub>2</sub>), aflatoxin G<sub>1</sub> (AFG<sub>1</sub>), zearalenone (ZEN), citrinin (CIT), FB<sub>1</sub>, and ochratoxin A (OTA) were purchased from Huaan Magnech Bio-Tech Co., Ltd. (Beijing, China). Oleylamine, sodium dodecyl sulfonate (SDS), gold(III) chloride hydrate, trisodium citrate (Na<sub>3</sub>C<sub>6</sub>H<sub>5</sub>O<sub>7</sub>·2H<sub>2</sub>O), bovine serum albumin (BSA), 1-ethyl-3-(3-dimethylaminopropyl) carbodiimide (EDC), and poly (maleicanhydride-alt-1-octadecene) (PMAO, MW = 30,000~50,000 Da) were obtained from Sigma-Aldrich (St. Louis, MO, USA). Anti-FB<sub>1</sub> monoclonal antibodies (mAbs) were kindly provided by prof. Yang Xu from Nanchang University (Nanchang, China). The BSA-FB<sub>1</sub> conjugates (molar ratio of 1:23) were prepared by our laboratory. The sample pad, the absorbent pad, and the NC membrane were provided by Wuxi Zodolabs Biotech Co., Ltd. (Jiangsu, China). Goat anti-mouse IgG was obtained from Chongqing Xinyuanjiahe Biotechnology Inc. (Chongqing, China). Other chemicals were of analytical grade and purchased from Sinopharm Chemical Corp. (Shanghai, China). All reagents were used without further purification.

### 2.2. Characterization

The morphology and structure of the prepared GNBs were investigated using a JEOL JEM 2100 transmission electron microscope (TEM, Tokyo, Japan). Dynamic light scattering (DLS) analysis was performed using a Zetasizer Nano-ZEN3700 instrument (Malvern, UK) to determine the size distribution of various GNBs. Ultraviolet–visible (UV–Vis) absorption spectra were obtained using an Amersham Pharmacia Ultrospec 4300 pro UV/visible spectrophotometer (England, UK). Real corn samples were fired by using a LC-Q/TOF MS instrument (Agilent 1290-6538, Palo Alto, CA, USA).

### 2.3. Synthesis of Hydrophobic AuNPs

Hydrophobic AuNPs with a size of 10 nm were prepared following a previous report [36]. In a typical synthesis procedure, gold(III) chloride hydrate (0.3 mmol) was dissolved in a mixed solution of oleylamine (7.4 mmol) and chloroform (1.0 mL) under magnetic stirring. The above-mentioned mixture was quickly added to 49 mL boiling chloroform solution containing 35.3 mmol oleylamine. After approximately 10 min, the color of the reaction solution became deep red. After continuous reaction for 3 h, the synthesized AuNPs were then collected by adding 50 mL ethanol. Finally, the hydrophobic AuNPs were stored in chloroform for further use.

### 2.4. Synthesis of Carboxylated GNBs

GNB<sub>129</sub> was prepared according to a previous work with a slight modification [30]. In a typical synthesis procedure, a 50 µL chloroform solution containing hydrophobic AuNPs (10 mg) and PMAO (2 mg) was added into 500 µL sodium dodecyl sulfate (SDS) solution (12 mg/mL), followed by ultrasonication for 2 min under 76.8 W ultrasonic power to produce an oil-in-water microemulsion. After the evaporation of chloroform at 60 °C for 2 h, the synthesized GNB<sub>129</sub> was centrifuged and then re-suspended in 0.01 M phosphate buffer (PB, pH 10) for 24 h to hydrolyze the anhydride group of PMAO into the carboxyl group. Finally, the resultant carboxylated GNB<sub>129</sub> was centrifuged and washed thrice with water. Similar synthesis procedures were conducted for preparing GNB<sub>94</sub> and GNB<sub>237</sub> but with alteration of the SDS amount and the volume ratio of oil/water (Table S1).

### 2.5. Synthesis of Anti-FB<sub>1</sub> Monoclonal Antibodies Labeled GNB<sub>129</sub> (GNB<sub>129</sub>-mAbs)

GNB<sub>129</sub>-mAbs were prepared through the formation of a peptide bond between the carboxyl group of GNB<sub>129</sub> and the amino group of antibodies by using the active ester method. Approximately 1  $\mu$ L anti-FB<sub>1</sub> mAbs (6.4 mg/mL) was added into 400  $\mu$ L 0.01 M pH 6.5 phosphate buffer (PB) solution containing GNB<sub>129</sub> (0.14 pM) and 1-ethyl-3-(3-dimethylamino) propyl carbodiimide (EDC) (1  $\mu$ g). The mixed solution was incubated for 90 min at room temperature. Subsequently, 10 mg BSA was added into the mixture solution for another 1 h of reaction. The synthesized GNB<sub>129</sub>-mAbs were then centrifuged and resuspended in 200  $\mu$ L 0.01 M PB (pH 7.4) containing 25% sucrose, 1% bovine serum albumin (BSA), and 0.1% sodium azide.

### 2.6. Preparation of BSA-FB<sub>1</sub> Conjugate

The BSA-FB<sub>1</sub> conjugate was synthesized according to a previous work with minor modification [37]. In brief, 0.5 mg of FB<sub>1</sub> and 3 mg of BSA were dissolved in 500  $\mu$ L of MES buffer solution (molar ratio of FB<sub>1</sub> to BSA is 15:1). About 0.2 mg of EDC was added to the mixture, then the mixture was incubated on a shaker at room temperature for 1 h. Unreacted EDC and FB<sub>1</sub> were removed via 3 d of dialysis in 1 L of 0.01 M PBS (pH 7.4). The final BSA-FB<sub>1</sub> solution was collected, added with glycerin at the final concentration of 50%, and then stored in a refrigerator at  $-20$  °C.

### 2.7. Construction of GNB<sub>129</sub>-LFIA Test Strips

The GNB<sub>129</sub>-LFIA test strips were constructed according to our previous report with slight modifications [38]. Here, 0.66 mg/mL BSA-FB<sub>1</sub> conjugates and 0.5 mg/mL goat anti-mouse IgG were sprayed onto the nitrocellulose (NC) membrane as the test (T) and control (C) lines at the density of 0.6 mL/cm on a ZX1000 dispensing platform. The distance between two lines was 6.0 mm. The NC membrane was then vacuum-dried overnight at 37 °C. The other operations are the same.

### 2.8. Quantitative Procedure of GNB-LFIA for FB<sub>1</sub> Detection

Approximately 2  $\mu$ L GNB<sub>129</sub>-mAb probes (0.34 fmol) were premixed with 70  $\mu$ L sample standard solutions containing a series of different concentrations of FB<sub>1</sub> for incubation of 5 min. The mixture solution was then added to the sample well of the assembled strip. After reaction for 15 min, the optical intensities at the T and C lines (OD<sub>T</sub> and OD<sub>C</sub>, respectively) were recorded using a commercial HG-8 colloidal gold strip reader. The competitive inhibition curve was established by plotting the inhibition rate ( $B/B_0 \times 100\%$ ) against the logarithm FB<sub>1</sub> concentrations, where B<sub>0</sub> and B represent the OD<sub>T</sub>/OD<sub>C</sub> values of negative and positive samples, respectively.

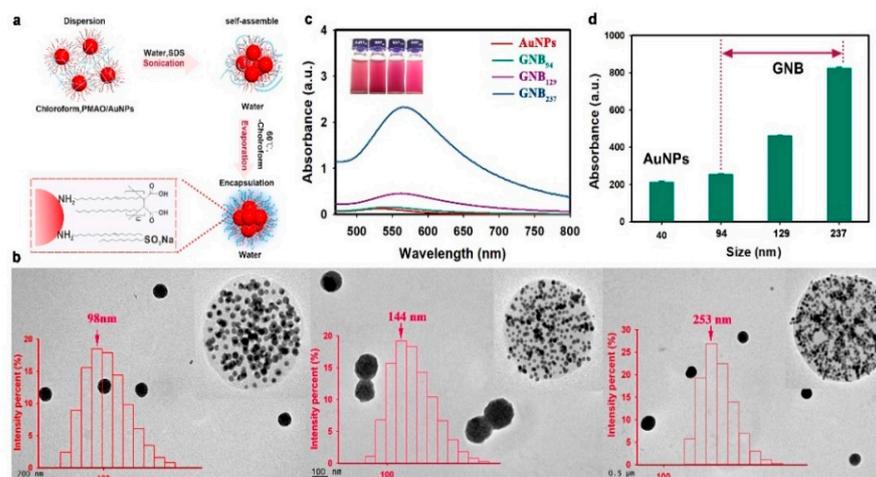
### 2.9. Sample Preparation

Real corn samples without FB<sub>1</sub> as confirmed by the liquid chromatography–mass spectrometry were purchased from the local supermarket. Briefly, the sample preparation and chromatography–mass spectrometry operation were performed according to the national standard GB5009.240-2016 (China). Thereafter, all the corn samples were spiked with FB<sub>1</sub> at a concentration ranging from 0.5 mg/kg to 10 mg/kg to evaluate the practicality of our designed GNB<sub>129</sub>-LFIA. Prior to LFIA detection, the FB<sub>1</sub> extraction was conducted as follows: 5.0 g FB<sub>1</sub>-contaminated pulverized corn sample was extracted with 4 mL methanol–water (60:40, *v/v*) for 20 min on a vortex shaker. After centrifugation at 16,000 rpm for 15 min, the supernatant was stored at  $-20$  °C and further diluted by 12-fold with 0.01 M pH 7.4 PB solution prior to analysis. To estimate the reliability of our method, we performed a correlation analysis between our GNB<sub>129</sub>-LFIA strip method and conventional enzyme-linked immunosorbent assay (ELISA) by simultaneously testing 35 real corn samples, with the FB<sub>1</sub> concentration ranging from 1.5 ng/mL to 267 ng/mL by using two approaches.

### 3. Results and Discussion

#### 3.1. Synthesis and Characterization of GNBs

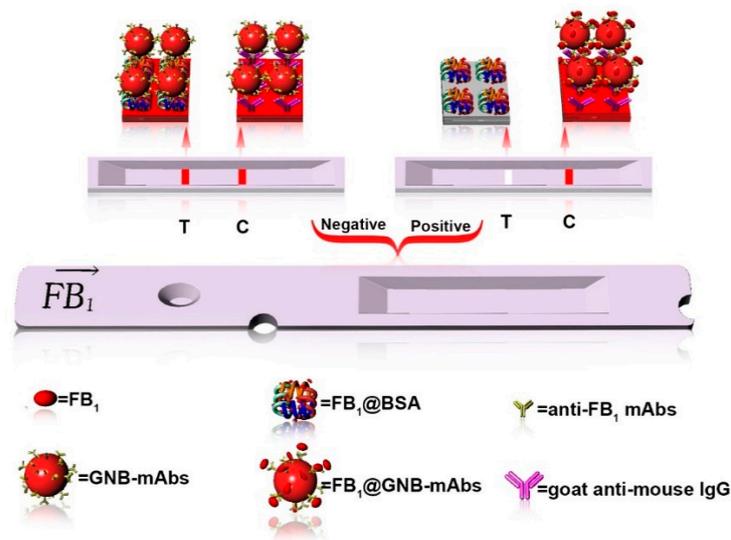
The GNBs were synthesized through the microemulsion-based self-assembly strategy. Figure 1a depicts the detailed synthetic procedure. Oleylamine-capped AuNPs (OA-AuNPs) with a size of 10 nm (Figure S1) were synthesized and used as building blocks for the self-assembled synthesis of GNBs. A mixed solution of OA-AuNPs and PMAO dissolved in chloroform was added to the SDS solution, followed by ultrasonic emulsification. The assembled GNBs were obtained with the evaporation of chloroform. Different sizes of GNBs were achieved by changing the SDS amount and the volume ratio of oil/water (Table S1). The resultant GNBs were then characterized by transmission electron microscopy (TEM), dynamic light scattering (DLS), and ultraviolet–visible (UV–vis) absorption spectra. The TEM images (Figure 1b) showed that all three assembled GNBs exhibited regular spheres measuring  $94 \pm 13$ ,  $129 \pm 17$ , and  $237 \pm 21$  nm, these values are slightly smaller than the hydrodynamic diameters measured by DLS (inset in Figure 1b), which were  $98 \pm 8$ ,  $144 \pm 12$ , and  $253 \pm 16$  nm, respectively. This variation may be due to the low contrast of the PMAO polymer layer on the GNB surface in TEM imaging. The magnified TEM image in the inset of Figure 1b indicates that numerous isolated AuNPs were successfully encapsulated into the polymer matrix. The embedded AuNP number increased with the increase in the GNB sizes. Figure 1c demonstrates that the UV–vis absorption spectra of the three GNBs obtained at the same particle concentration displayed the size-dependent increase in absorbance. The absorbance of GNB<sub>94</sub>, GNB<sub>129</sub>, and GNB<sub>237</sub> provided a 1.3-, 3.7-, and 17.7-fold enhancement compared with AuNP<sub>40</sub>. A red shift of GNBs from 542 nm to 556 nm was also observed, along with an evident color change from red to amaranth that is also suitable for the naked-eye-based detection (inset of Figure 1c). This result demonstrated that GNBs can provide a significant enhancement in absorbance but without compromising the naked-eye-based detection capability. GNBs of three sizes were sprayed onto the NC membrane as the T line to study their effect on the OD at the T area. The widely used AuNP<sub>40</sub> at the same particle concentration as GNBs was applied for direct comparison. The ODs were then recorded with a commercial HG-8 strip reader. Figure 1d also exhibits the size-dependent enhancement in OD values for GNBs, which are consistent with the change trend of absorbance against the GNB sizes. The OD values of GNB<sub>94</sub>, GNB<sub>129</sub>, and GNB<sub>237</sub> presented a 1.24-, 2.46-, and 4.08-fold enhancement compared with the AuNP<sub>40</sub>, respectively. These results illustrated that the assembled GNBs can provide remarkably enhanced colorimetric signal intensity on the test strip, thus contributing to the improvement of LFIA sensitivity.



**Figure 1.** (a) The synthetic route of the designed GNBs. (b) TEM images and DLS measurement. (c) UV-vis absorption spectra of GNB<sub>94</sub>, GNB<sub>129</sub>, GNB<sub>237</sub>, and AuNP<sub>40</sub>. (d) Comparison of the OD values by spraying the GNB<sub>94</sub>, GNB<sub>129</sub>, GNB<sub>237</sub>, and AuNP<sub>40</sub> on the NC membrane as the T lines at the same molar concentrations.

### 3.2. Detection Principle and Optimization of GNB-LFIA

Analogous to traditional competitive LFIA, the developed GNB-LFIA shares the same detection principle (Scheme 1). In the absence of  $FB_1$ , the GNB-mAb probes were captured by the BSA- $FB_1$  conjugates to produce a clear red band at the T line. On the contrary, the GNB-mAb probes first specifically recognized and captured the target  $FB_1$  from the sample solution in the presence of  $FB_1$  to form the GNB-mAb- $FB_1$  complex, thus resulting in the decreased capture of GNB-mAbs at the T line. Consequently, the red band at the T line markedly decreased and disappeared. Thus, an inverse proportional relationship between the colored intensity at the T zone, that is,  $OD_T$ , and the  $FB_1$  concentration was obtained, which provided the possibility for  $FB_1$  quantitation. The presence of red band at the C line signifies the validity of the GNB-LFIA test strip. The  $OD_C$  value was applied as a reference to enable a reliable signal output by using the  $OD_T/OD_C$  ratio.

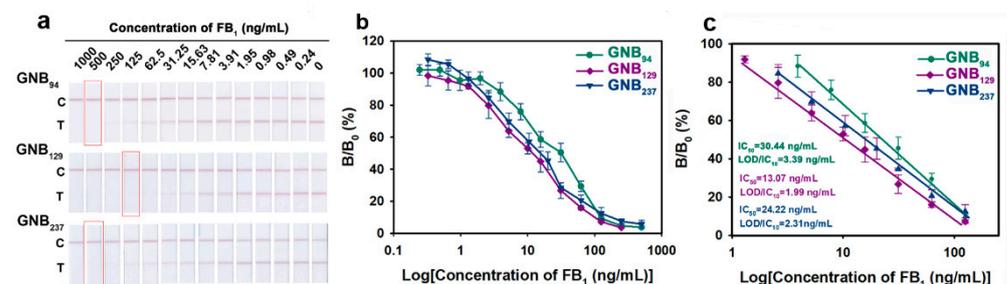


**Scheme 1.** Schematic illustration of the competitive GNB-LFIA for  $FB_1$  detection.

At present, the commonly used strategies for enhancing the detection sensitivity of competitive LFIA mainly include the following several aspects: (i) lowering the affinity of antibody to competing antigens; (ii) decreasing the amount of analytical antibody on the label; (iii) improving the signal intensity of the labeling probes; (iv) increasing the immunoreaction efficiency between the labeling probes and the antigen immobilized on the T line. The latter two approaches have attracted extensive research in recent years compared with the first method, which is often hard to perform for a pair of given antigen and antibody. In general, the signal intensity of the labeling probe is directly related to the probe size. For example, the absorbance and OD value increased with the increase in the GNB size. Such increment is theoretically beneficial to the improvement of the LFIA sensitivity. Nevertheless, the probe diffusion at the T line decreased with the increase in the probe size and reduced the immunoreaction efficiency, thus leading to sensitivity deterioration. The above-mentioned analysis manifested that the labeling probe with an appropriate size is crucial for the enhancement of the LFIA sensitivity. Thus, in this work, we first investigated the influence of the GNB size on the detection sensitivity of competitive LFIA. Several key factors, including the pH value, EDC concentration, and labeling concentration of anti- $FB_1$  mAbs, that affect the conjugation efficiency of antibody were systematically studied and optimized to obtain the three best GNB-mAb probes. The  $OD_T$  value obtained using the  $FB_1$ -negative sample and the competition inhibition rates  $((1 - B/B_0) \times 100\%)$  obtained using the  $FB_1$ -positive sample (20 ng/mL) were used to screen the optimum conditions. The results in Figures S2–S4 show that the optimal combinations are as follows: pH 6.0 for the three GNBs, EDC concentration of 0.625  $\mu\text{g/mL}$  for GNB<sub>94</sub> and GNB<sub>129</sub>, and 1.25  $\mu\text{g/mL}$  for GNB<sub>237</sub>; anti- $FB_1$  mAb concentration of

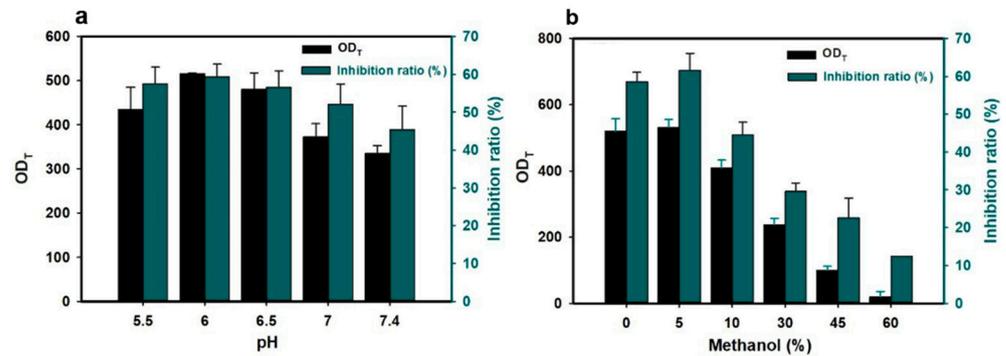
2.14  $\mu\text{g}$  per pmol for GNB<sub>94</sub>, 7.02  $\mu\text{g}$  for per pmol GNB<sub>129</sub>, and 36.8  $\mu\text{g}$  per pmol GNB<sub>237</sub>. Under these conditions, the appropriate OD<sub>T</sub> values were simultaneously obtained by using the blank sample and the highest inhibition rates for 20 ng/mL FB<sub>1</sub>. Further optimizations for the concentration of BSA-FB<sub>1</sub> sprayed on the T line and the amount of GNB-mAbs used in each strip were completed. The result in Tables S2–S4 revealed that the optimal selections for the used amounts of BSA-FB<sub>1</sub> and GNB-mAbs were as follows: 1.33 mg/mL BSA-FB<sub>1</sub> and 0.66 fmol GNB-mAbs for GNB<sub>94</sub>-LFIA, 1.33 mg/mL BSA-FB<sub>1</sub> and 0.34 fmol GNB-mAbs for GNB<sub>129</sub>-LFIA, and 1.33 mg/mL BSA-FB<sub>1</sub> and 0.18 fmol GNB-mAbs for GNB<sub>237</sub>-LFIA. Subsequently, the immunological kinetic analysis was performed by recording the changes in the OD<sub>T</sub>/OD<sub>C</sub> value against the immunoreaction time after running the strip using a PB saline (PBS) buffer containing the desired GNB-mAbs during a 30 min observation. Figure S5 shows that the OD<sub>T</sub>/OD<sub>C</sub> values for the three GNB-LFIA strips reached a plateau after 15 min of immunoreaction. This finding suggests that no significant difference exists in the immunoreaction kinetics at different sizes of GNBs. Thus, 15 min was selected as the optimal signal interpretation time for three GNB-LFIA strips.

Under the optimized condition, the detection performance of three GNB-LFIA strips was evaluated by simultaneously measuring a series of FB<sub>1</sub>-spiked PBS solutions with different target concentrations ranging from 0 ng/mL to 1000 ng/mL by using the developed three GNB-LFIA strips. Figure 2a shows the strip photographs obtained at different FB<sub>1</sub> concentrations. The results indicated that the cutoff values representing the concentrations of FB<sub>1</sub> that cause no color on the T line observed by the naked eye were 500 ng/mL for GNB<sub>94</sub>-LFIA, 125 ng/mL for GNB<sub>129</sub>-LFIA, and 500 ng/mL for GNB<sub>237</sub>-LFIA [6,39]. Figure 2b presents the concentration–response relationships from the three GNB-LFIA strips. The figure exhibits the similar concentration-dependent decrease in the B/B<sub>0</sub> × 100% for the three strips. The competitive inhibition (IC) curves for the three GNB-LFIA strips were further constructed by plotting the B/B<sub>0</sub> × 100% against the logarithmic FB<sub>1</sub> concentration. Figure 2c demonstrates that the GNB<sub>129</sub>-LFIA achieved a low IC<sub>50</sub> value of 13.07 ng/mL, which is 2.32- and 1.85-fold lower than those of GNB<sub>94</sub>-LFIA (IC<sub>50</sub>: 30.44 ng/mL) and GNB<sub>237</sub>-LFIA (IC<sub>50</sub>: 24.22 ng/mL). The OD<sub>T</sub> value of GNB<sub>237</sub> in Figure 1d is 1.66-fold higher than that of GNB<sub>129</sub>. However, the OD<sub>T</sub> of GNB<sub>237</sub>-LFIA is 1.85-fold lower than that of GNB<sub>129</sub>-LFIA in terms of sensitivity. These results demonstrated that the GNB size is a critical factor in enhancing the LFIA sensitivity; only appropriately sized GNBs can provide enhanced target detection. The possible reasons are as follows. (1) The small-size GNBs exhibited insufficient signal intensity, thus increasing the accumulated number of GNB at the T line for decreased competition and poor sensitivity; (2) the oversized GNBs displayed sufficient signal intensity but reduced diffusion and increased steric hindrance, causing low immunoreaction efficiency and sensitivity. Considering the high sensitivity, GNB<sub>129</sub>-LFIA was selected for all succeeding evaluation.



**Figure 2.** Effect of the GNB size on the detection sensitivity of competitive LFIA. (a) The prototypes of three GNB-LFIA strips responding to varying FB<sub>1</sub> concentrations. (b) The relationship analyses for three GNB-LFIAs between the B/B<sub>0</sub> × 100% value and the FB<sub>1</sub> concentration ranged from 0 to 1000 ng/mL. (c) The linear dependence of three GNB-LFIA strips obtained by plotting the B/B<sub>0</sub> × 100% against the logarithmic FB<sub>1</sub> concentration.

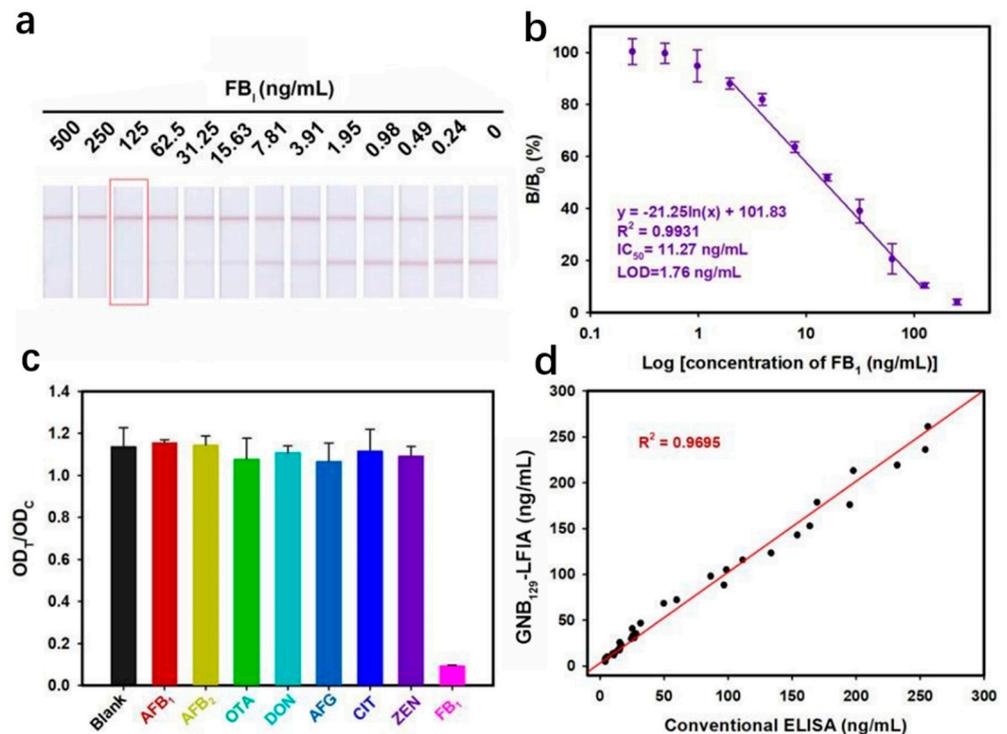
Previous studies demonstrated that the pH and methanol content in the reaction system are key parameters that could influence the sensitivity and reproducibility of LFIA by disturbing the antigen–antibody interaction. Thus, a careful investigation about the effects of pH and methanol concentration on the sensitivity of GNB<sub>129</sub>-LFIA was completed (Figure 3a,b). Results showed the optimized pH and methanol concentration at 6.0 and 5%, respectively.



**Figure 3.** Effect of the pH value (a) and methanol concentration (b) in the reaction system on the OD<sub>T</sub> value using the blank corn extraction solution and the competitive inhibition rate using the FB<sub>1</sub>-spiked corn extraction solution (20 ng/mL). The competitive inhibition rate was defined as  $(1 - B/B_0) \times 100\%$ , where B<sub>0</sub> and B represent the OD<sub>T</sub>/OD<sub>C</sub> value of the FB<sub>1</sub>-negative and positive sample, respectively.

### 3.3. Performance Evaluation of GNB<sub>129</sub>-LFIA for FB<sub>1</sub> in Corn Samples

Under the developed conditions, the calibration curve of the GNB<sub>129</sub>-LFIA strip was constructed by plotting  $B/B_0 \times 100\%$  against the logarithmic concentration of FB<sub>1</sub> in spiked corn samples. Figure 4a shows the strip photographs obtained at different FB<sub>1</sub> concentrations in real corn sample detection. Figure 4b presents that the  $B/B_0 \times 100\%$  value decreased as the FB<sub>1</sub> concentration increased. An excellent linear dependence was observed between the two factors at FB<sub>1</sub> concentration ranging from 3.9 ng/mL to 125 ng/mL with an R<sup>2</sup> of 0.9931. The regression equation can be described as  $y = -21.25\ln(x) + 101.83$ . The IC<sub>50</sub> value for FB<sub>1</sub> was as low as 11.27 ng/mL, which is 3.82-fold lower than that of the conventional AuNP<sub>40</sub>-based LFIA strip (IC<sub>50</sub> = 43.04 ng/mL) (Figure S6 and S7), and the LOD of GNB<sub>129</sub>-LFIA was as low as 1.79 ng/mL, according to 10% FB<sub>1</sub> competitive inhibition concentration, which was 2.89-fold lower than AuNP<sub>40</sub>-based LFIA [39]. The specificity analysis in Figure 4c suggested the excellent selectivity of this GNB<sub>129</sub>-LFIA strip for FB<sub>1</sub> against other common mycotoxins, including AFB<sub>1</sub>, AFB<sub>2</sub>, OTA, DON, AFG, CIT, and ZEN at the concentration of 1 μg/mL. The accuracy and precision analysis of this strip method was performed by calculating the intra- and inter-assay recoveries and coefficients of variation (CV) of the five FB<sub>1</sub>-spiked corn samples with FB<sub>1</sub> concentrations of 10, 5, 2, 1, and 0.5 mg/kg. Table 1 illustrates that the average recoveries for intra- and inter-assay changed from 91.42% to 112.64%, with the CV ranging from 5.16% to 15.6%, demonstrating an acceptable accuracy and precision for FB<sub>1</sub> quantification. The reliability of our method was further evaluated by detecting FB<sub>1</sub> in 35 spiked corn samples. The detection results were then compared with the well-accepted FB<sub>1</sub> ELISA kit method. The results in Figure 4d revealed that a high linear dependence with an R<sup>2</sup> of 0.9695 was achieved between the two approaches. This finding suggests that the developed GNB<sub>129</sub>-LFIA strip is comparable to ELISA in terms of FB<sub>1</sub> quantification. The proposed strip method is simple (no wash) and fast (15 min vs. 45 min for ELISA, in Figure S8) for the FB<sub>1</sub> screening test. Compared with other previously reported LFIA methods for measuring FB<sub>1</sub>, the prepared GNB<sub>129</sub>-LFIA possesses an acceptable sensitivity and quantitative linear range (Table S5).



**Figure 4.** The performance evaluation for the GNB<sub>129</sub>-LFIA strips for FB<sub>1</sub> detection in corn sample. (a) The prototypes of GNB<sub>129</sub>-LFIA strips responding to varying FB<sub>1</sub> concentrations in real corn sample detection. (b) The competitive inhibition curve of the GNB<sub>129</sub>-LFIA constructed by plotting the  $B/B_0 \times 100\%$  against the logarithm of FB<sub>1</sub> concentration. (c) The selectivity of our method by detecting the response against other common mycotoxins. (d) The correlation analysis of the detection results between the GNB<sub>129</sub>-LFIA strip and the ELISA method in 35 real corn samples, with FB<sub>1</sub> concentrations ranged from 1.5 to 267 ng/mL.

**Table 1.** The accuracy and precision of the GNB<sub>129</sub>-LFIA method for FB<sub>1</sub> detection in spiked corn samples.

Spiked Concentration FB <sub>1</sub> (mg kg <sup>-1</sup> )	Intra-Assay Precision			Inter-Assay Precision		
	Detected Concentration <sup>a</sup>	CV	Recovery (%)	Detected Concentration <sup>b</sup>	CV	Recovery (%)
10	9.78 ± 1.52	15.6	97.82	9.24 ± 0.39	5.16	92.43
5	5.63 ± 0.39	6.96	112.64	5.23 ± 0.47	7.37	112.5
2	1.94 ± 0.24	12.51	97.01	2.18 ± 0.21	9.80	108.97
1	0.97 ± 0.06	7.12	96.93	0.91 ± 0.09	9.40	91.42
0.5	0.48 ± 0.02	7.62	95.97	0.447 ± 0.03	5.30	89.41

<sup>a</sup> The assay was carried out in triplicates on the same day. <sup>b</sup> The assay was performed on three consecutive days.

#### 4. Conclusions

In this work, novel self-assembled GNBs were successfully synthesized by encapsulating hydrophobic AuNPs into a polymer matrix by using the emulsion-based self-assembly strategy. The obtained GNBs possessed a remarkably enhanced optical absorption, which is mainly attributed to the collective molar extinctions of numerous AuNPs embedded in GNBs. Using the designed GNBs as signal reporter, we further demonstrated that the developed GNB-LFIA can achieve the best detection for FB<sub>1</sub> in corn samples with an IC<sub>50</sub> of as low as 11.27 ng/mL under the optimal GNB size of 129 nm. The IC<sub>50</sub> value of our GNB<sub>129</sub>-LFIA was 3.82 times better than that of conventional AuNP<sub>40</sub>-LFIA. This work proves the feasibility of using the amplified GNBs as alternative probes to improve the

sensitivity of competitive LFIA. This study also provides a universal strategy to achieve enhanced target detection on conventional LFIA platform.

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## References

- Loynachan, C.N.; Thomas, M.R.; Gray, E.R.; Richards, D.A.; Kim, J.; Miller, B.S. Platinum Nanocatalyst Amplification: Redefining the Gold Standard for Lateral Flow Immunoassays with Ultrabroad Dynamic Range. *ACS Nano* **2018**, *12*, 279–288. [[CrossRef](#)] [[PubMed](#)]
- Pan, M.; Ma, T.; Yang, J.; Li, S.; Liu, S.; Wang, S. Development of Lateral Flow Immunochromatographic Assays Using Colloidal Au Sphere and Nanorods as Signal Marker for the Determination of Zearalenone in Cereals. *Foods* **2020**, *3*, 281. [[CrossRef](#)]
- Zhou, Y.; Ding, L.; Wu, Y.; Huang, X.; Lai, W.; Xiong, Y. Emerging Strategies to Develop Sensitive AuNP-Based ICTS Nanosensors. *TrAC Trends Anal. Chem.* **2019**, *112*, 147–160. [[CrossRef](#)]
- Luo, K.; Hu, L.; Guo, Q.; Wu, C.; Wu, S.; Liu, D. Comparison of 4 Label-Based Immunochromatographic Assays for the Detection of Escherichia Coli O157:H7 in Milk. *J. Dairy Sci.* **2017**, *100*, 5176–5187. [[CrossRef](#)] [[PubMed](#)]
- Khlebtsov, B.N.; Tumskiy, R.S.; Burov, A.M.; Pylaev, T.E.; Khlebtsov, N.G. Quantifying the Numbers of Gold Nanoparticles in the Test Zone of Lateral Flow Immunoassay Strips. *ACS Appl. Nano Mater.* **2019**, *2*, 5020–5028. [[CrossRef](#)]
- Duan, H.; Huang, X.; Shao, Y.; Zheng, L.; Guo, L.; Xiong, Y. Size-Dependent Immunochromatographic Assay with Quantum Dot Nanobeads for Sensitive and Quantitative Detection of Ochratoxin A in Corn. *Anal. Chem.* **2017**, *89*, 7062–7068. [[CrossRef](#)]
- Zhao, P.; Wu, Y.; Zhu, Y.; Yang, X.; Jiang, X.; Xiao, J. Upconversion Fluorescent Strip Sensor for Rapid Determination of *Vibrio Anguillarum*. *Nanoscale* **2014**, *6*, 3804–3809. [[CrossRef](#)] [[PubMed](#)]
- Sun, Q.; Zhao, G.; Dou, W. An Optical and Rapid Sandwich Immunoassay Method for Detection of Salmonella Pullorum and Salmonella Gallinarum Based on Immune Blue Silica Nanoparticles and Magnetic Nanoparticles. *Sens. Actuators B* **2016**, *226*, 69–75. [[CrossRef](#)]
- Huang, Z.; Hu, S.; Xiong, Y.; Wei, H.; Xu, H.; Duan, H.; Lai, W. Application and Development of Superparamagnetic Nanoparticles in Sample Pretreatment and Immunochromatographic Assay. *TrAC Trends Anal. Chem.* **2019**, *114*, 151–170. [[CrossRef](#)]
- Dement'eva, O.; Naumova, K.; Zhigletsova, S.; Klykova, M.; Somov, A.; Dunaytsev, I.; Senchikhin, I.; Volkov, V.; Rudoy, V. Drug-Templated Mesoporous Silica Nanocontainers with Extra High Payload and Controlled Release Rate. *Colloids Surf. B.* **2020**, *185*, 110577. [[CrossRef](#)]
- Gómez-Hens, A.; Manuel Fernández-Romero, J. The Role of Liposomes in Analytical Processes. *TrAC Trends Anal. Chem.* **2005**, *24*, 9–19. [[CrossRef](#)]
- Slowing, I.I.; Trewyn, B.G.; Giri, S.; Lin, V.S.Y. Mesoporous Silica Nanoparticles for Drug Delivery and Biosensing Applications. *Adv. Funct. Mater.* **2007**, *17*, 1225–1236. [[CrossRef](#)]
- Hofmann, C.; Duerkop, A.; Baeumner, A.J. Nanocontainers for Analytical Applications. *Angew. Chem. Int. Ed.* **2019**, *58*, 12840–12860. [[CrossRef](#)]
- Bhushan, B.; Kumar, S.U.; Matai, I.; Sachdev, A.; Dubey, P.; Gopinath, P. Ferritin Nanocages: A Novel Platform for Biomedical Applications. *J. Biomed. Nanotechnol.* **2014**, *10*, 2950–2976. [[CrossRef](#)]
- Feng, A.; Yuan, J. Smart Nanocontainers: Progress on Novel Stimuli-Responsive Polymer Vesicles. *Macromol. Rapid Commun.* **2014**, *35*, 767–779. [[CrossRef](#)] [[PubMed](#)]
- Li, W.; Wu, X.; Han, N.; Chen, J.; Qian, X.; Deng, Y.; Tang, W.; Chen, Y. MOF-Derived Hierarchical Hollow ZnO Nanocages with Enhanced Low-Concentration VOCs Gas-Sensing Performance. *Sens. Actuators B* **2016**, *225*, 158–166. [[CrossRef](#)]

17. Bi, J.; Wang, H.; Kamal, T.; Zhu, B.-W.; Tan, M. A Fluorescence Turn-Off-On Chemosensor Based on Carbon Nanocages for Detection of Ascorbic Acid. *RSC Adv.* **2017**, *7*, 30481–30487. [[CrossRef](#)]
18. Misson, M.; Zhang, H.; Jin, B. Nanobiocatalyst Advancements and Bioprocessing Applications. *J. R. Soc. Interface* **2015**, *12*, 20140891. [[CrossRef](#)] [[PubMed](#)]
19. Broz, P.; Driamov, S.; Ziegler, J.; Ben-Haim, N.; Marsch, S.; Meier, W.; Hunziker, P. Toward Intelligent Nanosize Bioreactors: A pH-Switchable, Channel-Equipped, Functional Polymer Nanocontainer. *Nano Lett.* **2006**, *6*, 2349–2353. [[CrossRef](#)] [[PubMed](#)]
20. Li, J.; Lu, S.; Huang, H.; Liu, D.; Zhuang, Z.; Zhong, C. ZIF-67 as Continuous Self-Sacrifice Template Derived NiCo<sub>2</sub>O<sub>4</sub>/Co,N-CNTs Nanocages as Efficient Bifunctional Electrocatalysts for Rechargeable Zn–Air Batteries. *ACS Sustain. Chem. Eng.* **2018**, *6*, 10021–10029. [[CrossRef](#)]
21. Trantidou, T.; Friddin, M.; Elani, Y.; Brooks, N.J.; Law, R.V.; Seddon, J.M.; Ces, O. Engineering Compartmentalized Biomimetic Micro- and Nanocontainers. *ACS Nano* **2017**, *11*, 6549–6565. [[CrossRef](#)] [[PubMed](#)]
22. Wang, Y.; Han, P.; Xu, H.; Wang, Z.; Zhang, X.; Kabanov, A.V. Photocontrolled Self-Assembly and Disassembly of Block Ionomer Complex Vesicles: A Facile Approach toward Supramolecular Polymer Nanocontainers. *Langmuir* **2010**, *26*, 709–715. [[CrossRef](#)]
23. Haase, M.F.; Grigoriev, D.O.; Möhwald, H.; Shchukin, D.G. Development of Nanoparticle Stabilized Polymer Nanocontainers with High Content of the Encapsulated Active Agent and Their Application in Water-Borne Anticorrosive Coatings. *Adv. Mater.* **2012**, *24*, 2429–2435. [[CrossRef](#)]
24. Yagai, S.; Karatsu, T.; Kitamura, A. Photocontrollable Self-Assembly. *Chem. Eur. J.* **2005**, *11*, 4054–4063. [[CrossRef](#)] [[PubMed](#)]
25. O’Neil, C.P.; Suzuki, T.; Demurtas, D.; Finka, A.; Hubbell, J.A. A Novel Method for the Encapsulation of Biomolecules into Polymersomes via Direct Hydration. *Langmuir* **2009**, *25*, 9025–9029. [[CrossRef](#)]
26. Lo, H.; Ponticciello, M.S.; Leong, K.W. Fabrication of Controlled Release Biodegradable Foams by Phase Separation. *Tissue Eng.* **1995**, *1*, 15–28. [[CrossRef](#)] [[PubMed](#)]
27. Capadona, J.R.; Van Den Berg, O.; Capadona, L.A.; Schroeter, M.; Rowan, S.J. A Versatile Approach for the Processing of Polymer Nanocomposites with Self-Assembled Nanofibre Templates. *Nat. Nanotechnol.* **2007**, *2*, 765–769. [[CrossRef](#)]
28. Messenger, L.; Burns, J.R.; Kim, J.; Cecchin, D.; Hindley, J.; Pyne, A.L.; Gaitzsch, J.; Battaglia, G.; Howorka, S. Biomimetic Hybrid Nanocontainers with Selective Permeability. *Angew. Chem.* **2016**, *128*, 11272–11275. [[CrossRef](#)]
29. Ren, M.; Xu, H.; Huang, X.; Kuang, M.; Xiong, Y.; Xu, H.; Xu, Y.; Chen, H.; Wang, A. Immunochromatographic Assay for Ultrasensitive Detection of Aflatoxin B1 in Maize by Highly Luminescent Quantum Dot Beads. *ACS Appl. Mater. Interfaces* **2014**, *6*, 14215–14222. [[CrossRef](#)]
30. Chen, X.; Leng, Y.; Hao, L.; Duan, H.; Yuan, J. Self-Assembled Colloidal Gold Superparticles to Enhance the Sensitivity of Lateral Flow Immunoassays with Sandwich Format. *Theranostics* **2020**, *10*, 3737–3748. [[CrossRef](#)]
31. Zhan, L.; Guo, S.-Z.; Song, F.; Gong, Y.; Xu, F.; Boulware, D.R.; McAlpine, M.C.; Chan, W.C.W.; Bischof, J.C. The Role of Nanoparticle Design in Determining Analytical Performance of Lateral Flow Immunoassays. *Nano Lett.* **2017**, *17*, 7207–7212. [[CrossRef](#)]
32. Petrarca, M.H.; Rodrigues, M.I.; Rossi, E.A.; de Sylos, C.M. Optimisation of A Sample Preparation Method for the Determination of Fumonisin B1 in Rice. *Food Chem.* **2014**, *158*, 270–277. [[CrossRef](#)] [[PubMed](#)]
33. Mexía-Salazar, A.L.; Hernández-López, J.; Burgos-Hernández, A.; Cortez-Rocha, M.O.; Castro-Longoria, R.; Ezquerro-Brauer, J.M. Role of Fumonisin B1 on the Immune System, Histopathology, and Muscle Proteins of White Shrimp (*Litopenaeus Vannamei*). *Food Chem.* **2008**, *110*, 471–479. [[CrossRef](#)] [[PubMed](#)]
34. Wang, Z.; Li, H.; Li, C.; Yu, Q.; Shen, J.; De Saeger, S. Development and Application of a Quantitative Fluorescence-Based Immunochromatographic Assay for Fumonisin B1 in Maize. *J. Agric. Food Chem.* **2014**, *62*, 6294–6298. [[CrossRef](#)] [[PubMed](#)]
35. Anttila, A.; Bhat, R.V.; Bond, J.A.; Borghoff, S.J.; Bosch, F.X.; Carlson, G.P.; Castegnaro, M.; Cruzan, G.; Gelderblom, W.C.; Hass, U. IARC Monographs on the Evaluation of Carcinogenic Risks to Humans: Some Traditional Herbal Medicines, Some Mycotoxins, Naphthalene and Styrene. In *IARC Monographs on the Evaluation of Carcinogenic Risks to Humans*; IARC Press: Lyon, France, 2002; Volume 82.
36. Hiramatsu, H.; Osterloh, F.E. A Simple Large-Scale Synthesis of Nearly Monodisperse Gold and Silver Nanoparticles with Adjustable Sizes and with Exchangeable Surfactants. *Chem. Mater.* **2004**, *16*, 2509–2511. [[CrossRef](#)]
37. Chen, X.; Liang, Y.; Zhang, W.; Leng, Y.; Xiong, Y. A Colorimetric Immunoassay Based on Glucose Oxidase-Induced AuNP Aggregation for Fumonisin B1. *Talanta* **2018**, *186*, 29–35. [[CrossRef](#)]
38. Ji, Y.; Ren, M.; Li, Y.; Huang, Z.; Shu, M.; Yang, H.; Xiong, Y.; Xu, Y. Detection of Aflatoxin B1 with Immunochromatographic Test Strips: Enhanced Signal Sensitivity using Gold Nanoflowers. *Talanta* **2015**, *142*, 206–212. [[CrossRef](#)]
39. Duan, H.; Chen, X.; Xu, W.; Fu, J.; Xiong, Y.; Wang, A. Quantum-Dot Submicrobead-Based Immunochromatographic Assay for Quantitative and Sensitive Detection of Zearalenone. *Talanta* **2015**, *132*, 126–131. [[CrossRef](#)] [[PubMed](#)]