



Electronic Supporting Information:

Cyclodextrin Cationic Polymer-based Nanoassemblies to Manage Inflammation by Intra-articular Delivery Strategies

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1. PolyCD

We estimated 15 CD cavities on the polymer network (PolyCD, Average MW = 25 kDa, CD content ~70%) and 0.21 mmol/g of amino groups. The amount of amino groups was spectroscopically estimated by the colorimetric Kaiser Test [1,2], according to the following equation:

$$NH_2 \text{ loading (mmol/g)} = \frac{[Abs_{sample} - Abs_{blank}] \times dilution (mL) \times 10^3}{\epsilon (M^{-1}cm^{-1}) \times sample \text{ weight (mg)} \times optical \text{ path (cm)}} \quad (1)$$

where Abs_{sample} is the absorbance at absorption maximum due to the amino groups of the PolyCD sample ($\lambda_{max} = 574 \text{ nm}$), Abs_{blank} was measured at the same conditions but without PolyCD. Dilution was fixed to 5 mL and extinction coefficient (ϵ) at 574 nm was $15,000 \text{ M}^{-1} \text{ cm}^{-1}$. Optical path was 0.5 cm.

2 Analysis of release kinetic

The kinetic analysis (Table 3, main text) was performed using three different models proposed in the literature by Higuchi, Baker-Lonsdale and a simple first order process (described in the main text). The first model describes drug release from the matrix as a square root of a time dependent process based on Fickian diffusion. It is possible to resume the Higuchi model with the following expression (generally known as the simplified Higuchi model):

$$C_t = k_H t^{\frac{1}{2}} \quad (2)$$

where C_t is the amount of the drug released (in percentage) as function of time t and k_H is the Higuchi dissolution constant.

The Baker-Lonsdale model describes the drug controlled release from a spherical matrix, as follows:

$$\frac{3}{2} \left[1 - \left(1 - \frac{C_t}{C_\infty} \right)^{2/3} \right] - \frac{C_t}{C_\infty} = kt \quad (3)$$

where C_t and C_∞ are the amounts of drug released in the receiving phase (in percentage) at time t and t_∞ , respectively.

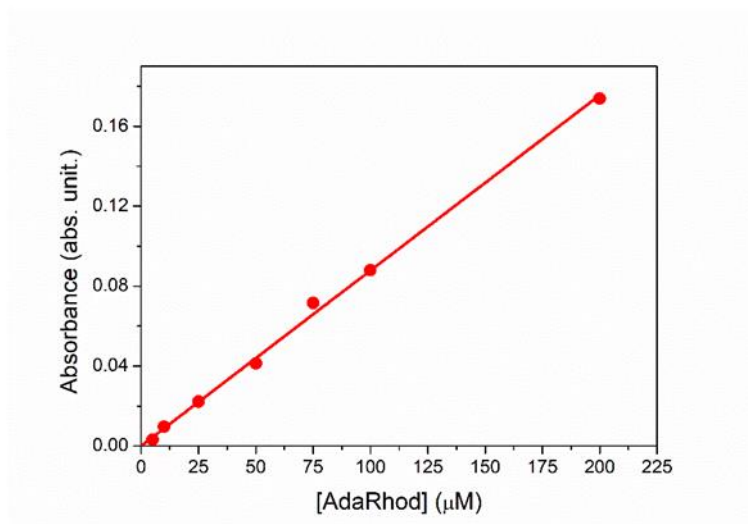


Figure S1. Determination of extinction coefficient by Lambert-Beer law of free Ada-Rhod in DCM at r.t.: $\epsilon_{\text{(Ada-Rhod)}} (\lambda_{\text{max}}=558 \text{ nm}) = 877.8 \pm 10 \text{ M}^{-1} \text{ cm}^{-1}$, ($R^2 = 0.99$).

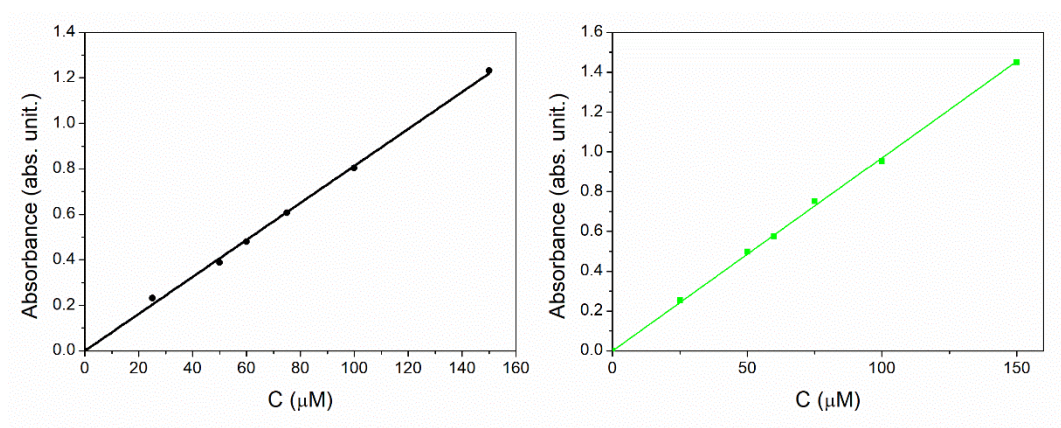


Figure S2. Determination of extinction coefficients by Lambert-Beer law: **A)** in ultrapure water (free DCF, black trace) at r.t.: $\epsilon_{\text{DCF}} (\lambda_{\text{max}}=276 \text{ nm}) = 8130 \pm 800 \text{ M}^{-1} \text{ cm}^{-1}$ ($R^2 = 0.99$); **B)** in PBS (free DCF, green trace) at r.t.: $\epsilon_{\text{DCF(PBS)}} (\lambda_{\text{max}}=276 \text{ nm}) = 9700 \pm 767 \text{ M}^{-1} \text{ cm}^{-1}$ ($R^2=0.99$).

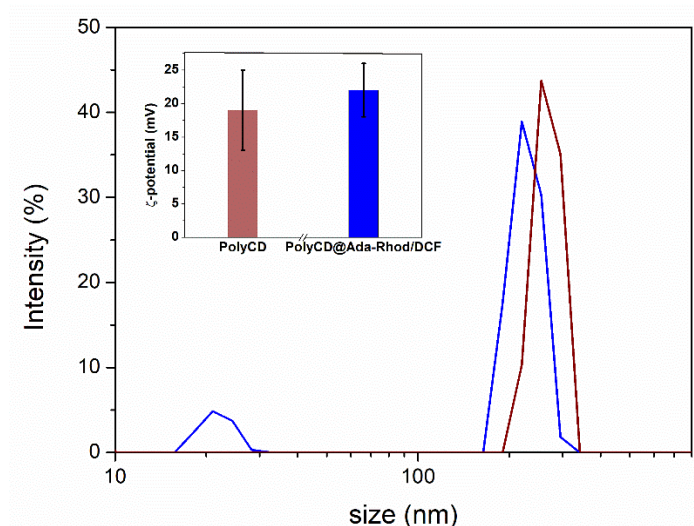


Figure S3. Size (or D_H) distribution of PolyCD (wine trace) and PolyCD@Ada-Rhod/DCF (blue trace) in ultrapure water. In the inset ζ potential $\pm$ SD of PolyCD (wine bar) and PolyCD@Ada-Rhod/DCF (blue bar). Experimental conditions: PolyCD and PolyCD@Ada-Rhod/DCF 0.5 mg/mL [DCF] = 236 μ M ; [Ada-Rhod] = 8 μ M, in ultrapure water at r.t.

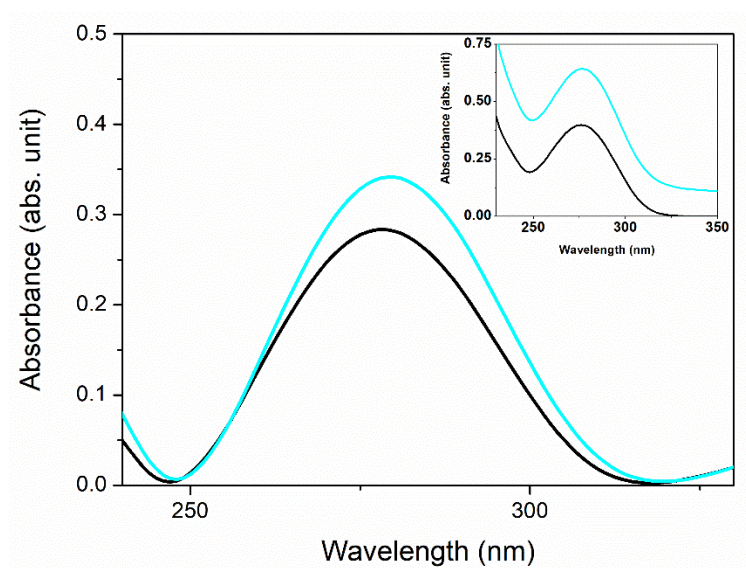


Figure S4. UV/Vis of free DCF (black trace) and PolyCD/DCF (cyan trace) in ultrapure water (scattering was subtracted) obtained by solvent evaporation technique. In the inset, spectra UV/Vis are reported without scattering subtraction. Experimental conditions: [CD] = [DCF] = 35 μ M; d = 1 cm, T = 25 $^{\circ}$ C.

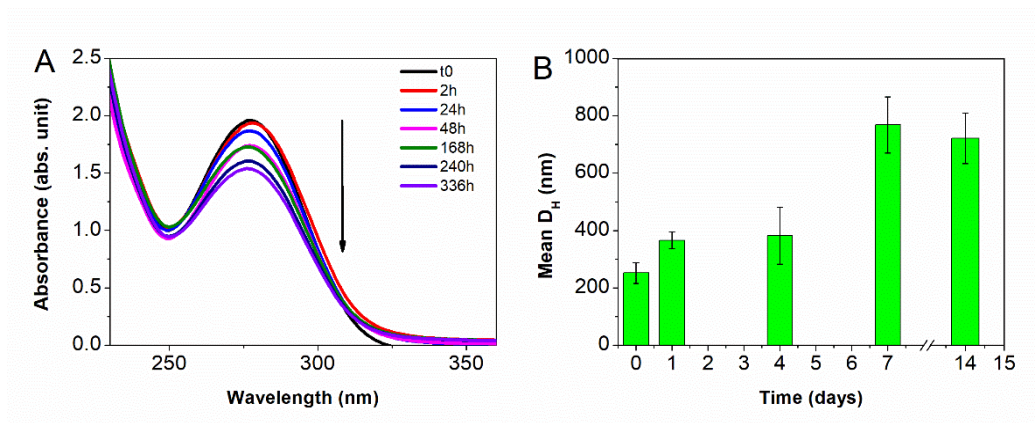


Figure S5. UV spectra (A) and mean D_H (B) (main populations only) vs time of PolyCD@Ada-Rhod/DCF nanoassemblies in NaCl wt. 0.9% (0.5 mg/mL, [Ada-Rhod] = 8 μ M, [DCF] = 236 μ M). Data were acquired at t = 0, 1, 4, 7 and 14 days. Nanoassembly dispersions were stored at 25 $^{\circ}$ C along the experimental time.

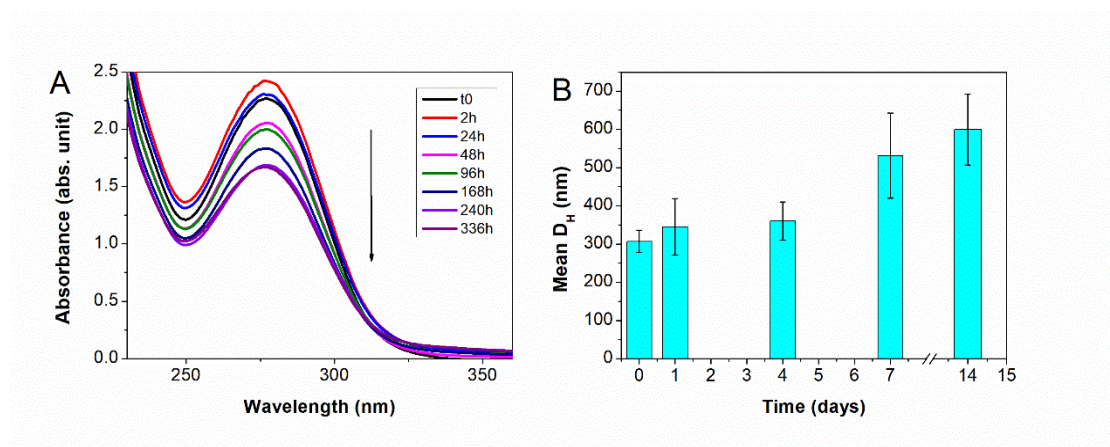


Figure S6. UV spectra (A) and mean D_H (B) (main populations only) vs time of PolyCD@Ada-Rhod/DCF nanoassemblies in in PBS (0.5 mg/mL, [Ada-Rhod] = 8 μ M, [DCF] = 236 μ M). Data were acquired at t = 0, 1, 4, 7 and 14 days. Nanoassembly dispersions were stored at 25 $^{\circ}$ C along the experimental time.

References

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