

Article



Very Large Pores Mesoporous Silica as New Candidate for Delivery of Big Therapeutics Molecules, Such as Pharmaceutical Peptides

Debora Carrozza 🔍, Gianluca Malavasi * 🗅 and Erika Ferrari 🗅

Department of Chemical and Geological Sciences, University of Modena and Reggio Emilia, Via G. Campi 103, 41125 Modena, Italy; debora.carrozza@unimore.it (D.C.); erika.ferrari@unimore.it (E.F.) * Correspondence: gianluca.malavasi@unimore.it

Abstract: The synthesis of a scaffold that can accommodate big molecules with a pharmaceutical role is important to shield them and maintain their biological activity. In this field, silica particles with large pores (LPMS) are innovative supports. Large pores allow for the loading of bioactive molecules inside the structure and contemporarily their stabilization and protection. These purposes cannot be achieved using classical mesoporous silica (MS, pore size 2–5 nm), because their pores are not big enough and pore blocking occurs. LPMSs with different porous structures are synthesized starting from an acidic water solution of tetraethyl orthosilicate reacting with pore agents (Pluronic[®] F127 and mesitylene), performing hydrothermal and microwave-assisted reactions. Time and surfactant optimization were performed. Loading tests were conducted using Nisin as a reference molecule (polycyclic antibacterial peptide, with dimensions of 4-6 nm); UV-Vis analyses on loading solutions were performed. For LPMSs, a significantly higher loading efficiency (LE%) was registered. Other analyses (Elemental Analysis, Thermogravimetric Analysis and UV-Vis) confirmed the presence of Nisin in all the structures and its stability when loaded on them. LPMSs showed a lower decrease in specific surface area if compared to MS; in terms of the difference in LE% between samples, it is explained considering the filling of pores for LPMSs, a phenomenon that is not allowed for MSs. Release studies in simulated body fluid highlight, only for LPMSs, a controlled release, considering the longer time scale of release. Scanning Electron Microscopy images acquired before and after release tests shows the LPMSs' maintenance of the structure, demonstrating strength and mechanical resistance of structures. In conclusion, LPMSs were synthesized, performing time and surfactant optimization. LPMSs showed better loading and releasing properties with respect to classical MS. All collected data confirm a pore blocking for MS and an in-pore loading for LPMS.

Keywords: large pores' mesoporous silica; Nisin; pharmaceutical peptides; porous biomaterials

1. Introduction

In the actual scenery, immunoresistance against viruses, bacteria and fungi plays a key role in the current scientific research. Antimicrobial peptides (AMPs) have attracted great attention as a potential substituent for conventional antibiotics [1,2]. This appends previous research because they have recently been targeted as novel antimicrobial agents with the potential to treat multiple drug-resistant infections [2,3]. For this reason, peptides with antimicrobial and anticancer activities could be a new pathway to follow [4–6].

The administration and the in situ delivery and release of peptides cannot be easily performed, because of their denaturation caused by peptidase present in biological fluids. In fact, AMPs can hardly survive in the environment of infected tissue and have poor physiochemical stability with a short circulating plasma half-life [1,7,8]. So, increasing the bioavailability or stability of peptide drugs through delivery or formulation is the key to the clinical applications of peptides [1,3,9].



Citation: Carrozza, D.; Malavasi, G.; Ferrari, E. Very Large Pores Mesoporous Silica as New Candidate for Delivery of Big Therapeutics Molecules, Such as Pharmaceutical Peptides. *Materials* **2023**, *16*, 4151. https://doi.org/10.3390/ma16114151

Academic Editor: Satoshi Komasa

Received: 10 May 2023 Revised: 29 May 2023 Accepted: 31 May 2023 Published: 2 June 2023



Copyright: © 2023 by the authors. Licensee MDPI, Basel, Switzerland. This article is an open access article distributed under the terms and conditions of the Creative Commons Attribution (CC BY) license (https:// creativecommons.org/licenses/by/ 4.0/). Following this philosophy, the synthesis of a scaffold that can accommodate these big molecules is important to shield them and maintain their biological activity [10]. Their conjugation with various classes of materials and their delivery via carrier systems are strategies being used to enhance their therapeutic efficacy.

In this field, silica particles with large pores (comparable to the peptides dimensions) are innovative and can provide interesting support [10]. In fact, large pores could allow for the loading of the bioactive molecule inside the structure and contemporarily allow for their stabilization and protection from peptidase [11]. These purposes cannot be achieved using classical mesoporous silica (MS, with pore size of 2–5 nm) [12], because their pores are not big enough to enable the insertion inside them, and only external loading can be performed [13]. Pores' size is an important aspect because it has been demonstrated [10] that the dependence of in vitro adsorption/release of AMPs is a function of the mesopores' size. Results obtained prove that the mesopores' size critically influences the encapsulation of AMPs, and at low concentrations, encapsulation can be achieved only for the structures in which mesopores' size are in the range of peptide dimensions.

Mesoporous silica can be synthesized starting from a solution containing the following: tetraethyl orthosilicate (TEOS), which is a silica structure precursor, a pore agent that can be tuned (in terms of quantity and type) according to pores' dimensions that you want to obtain and an adjuvant of pore agent that helps to obtain larger pores [14–16].

Furthermore, with the idea of obtaining smart materials, silica particles can be loaded with the pharmacologically bioactive molecule, and then the particles can be covered with an intelligent coating (sensible to variation of environmental potential, that occurs near the tumoral environment) that detaches from the surface and permits the in situ release of the drug [17–19].

The aim of this work was to find a new synthesis pathway for obtaining LPMS particles, with a high pores' dimension range; then, we performed the optimization of the synthesis in terms of surfactant used [20] and reaction time. Later, LPMSs were used as support for loading a peptide, and simultaneously, loadings were also performed into classical MS to have a comparison sample. Additionally, releases were performed for both LPMSs and MS. All results collected (SSA, TGA-DTA curves, UV-VIS analysis and EA) demonstrate a higher encapsulation of the peptide inside LPMSs and a controlled and longer release. SEM-FEG images acquired for LPMSs after release tests confirm the improvement of mechanical resistance and strength of the structure. Not so good results were obtained for MS, demonstrating that LPMSs are better candidates to be used as drug delivery systems of big therapeutic molecules.

2. Materials and Methods

2.1. General Procedures

All the chemicals and solvents were purchased with the highest purity grade available and used without further purification unless otherwise specified. To synthetized LPMSs, hydrothermal treatments were performed with microwaves (MWs), using FlexiWAVE (Milestone S.r.l., Sorisole, Italy) 230 V.

2.2. Synthesis of LPMSs

The synthesis of LPMS was adapted based on earlier studies [16,20]. In general, TEOS is used as silica structure precursor, where Pluronic surfactant is the pore agent and TMB is the adjuvant of surfactant.

In this work, to synthesize LPMSs, we started from an acidic water solution (1.7% w/w HCl) containing the following: tetraethyl orthosilicate (TEOS) (98%, Merck, Darmstadt, Germany), Pluronic[®] surfactant P123 or F127 (>99.9%, Merck, Darmstadt, Germany) and 1,2,3-Trimethylbenzene (TMB) (100%, Merck, Darmstadt, Germany). The solution was hydrothermally treated with MWs, starting with a thermal treatment at 80 °C for 6 h and then followed by a second thermal treatment at 160 °C for 12 h. MWs' power was dosed by the instrument based on the solution temperature.

Different molar ratios between TEOS and Pluronic were studied in addition to different reaction times. Furthermore, syntheses with and without TMB were performed to evaluate the effect of TMB on pores' dimensions.

All syntheses conducted are reported in Table 1. Samples were named as LPMS_n_TMB_yh, in which n is the chronological number of the synthesis, TMB indicates the presence or not of the adjuvant and y is the number of hours if it is different from 18 h (in these cases, the ratio between the times of treatment at 80 °C and 160 °C was maintained).

Sample	Type of Surfactant	Reaction Time (h)	Mass RatioSurfactantTEOS/Surfactant(g)		TEOS (g)	TMB (mL)	HCl (1.7%) <i>w/w</i> (mL)
LPMS_1_TMB_18h	P123	18	1.7	3.4	2.0	0.52	140
LPMS_2_TMB_18h	P123	18	1.7	3.4	2.0	0.26	140
LPMS_1_18h	P123	18	1.7	3.4	2.0	-	140
LPMS_2_18h	P123	18	1.7	3.4	2.0	-	140
LPMS_1_TMB_2h	P123	2	1.7	3.4	2.0	0.52	140
LPMS_1_TMB_4h	P123	4	1.7	3.4	2.0	0.52	140
LPMS_1_TMB_6h	P123	6	1.7	3.4	2.0	0.52	140
LPMS_1_TMB_8h	P123	8	1.7	3.4	2.0	0.52	140
LPMS_3_TMB_8h	P123	8	1.0	2.0	2.0	0.52	140
LPMS_4_TMB_8h	P123	8	1.4	2.8	2.0	0.52	140
LPMS_5_TMB_8h	P123	8	2.0	4.0	2.0	0.52	140
LPMS_6_TMB_18h	P123	18	2.0	4.0	2.0	0.52	140
LPMS_7_TMB_18h	F127	18	2.0	4.0	2.0	0.52	140
LPMS_8_TMB_8h	F127	8	2.0	4.0	2.0	0.52	140
LPMS_9_TMB_8h	F127	8	1.7	3.4	2.0	0.52	140
LPMS_10_TMB_8h	F127	8	1.4	2.0	2.0	0.52	140
LPMS_11_TMB_8h	F127	8	1.0	2.8	2.0	0.52	140

Table 1. Synthesis conducted.

After thermal treatment, synthesis solutions were filtered, the collected solids were dried overnight at 60 °C and then they were calcined at 2 °C/min up to 700 °C for 3 h, under an air atmosphere to remove the surfactant as well as to stabilize the resultant mesoporous glasses. After quenching in air, the LPMSs were gently milled in an agate mortar and sieved at a mean dimension lower than 355 μ m.

2.3. Loading Tests

Loading tests were conducted choosing a molecule able to discriminate between LPMS and MS pores. For this reason, loadings were performed with Nisin (Figure 1) (>900 IU/mg, min 50% NaCl, Biosynth, Nobelova, Slovakia), an antimicrobial and biocompatible peptide that is 5.6 nm big [21–23].

Different loading solution concentrations were studied (from 0.5 to 20 mg of Nisin per mL of deionized water). Loading tests were performed by soaking 125 mg of the sample with 5 mL of loading solution, in a thermos-shaker at 25 $^{\circ}$ C, 120 rpm for 24 h; after that, solutions were centrifuged, and the solids were collected, washed and treated at 70 $^{\circ}$ C overnight to remove water.

On dried solids, we performed Elemental Analysis to evaluate the Nisin content; therefore, Nisin solutions were collected to spectrophotometrically determine the Nisin content before and after soaking. Spectrophotometric quantification was performed using a Nisin calibration curve in a concentration range of 0.2–1 mg/mL of Nisin in deionized water.



Figure 1. Nisin structure.

2.4. Nisin Release in Simulated Body Fluid (SBF)

Dried solids were used to conduct Nisin release tests just after solid drying and after a few weeks to evaluate Nisin stability [24]. Dried solids were preserved in anhydrous and dark conditions, and both release tests gave same results. First, 50 mg of sample were soaked with 5 mL of SBF solution for different timing (from 0.5 up to 96 h) in a thermosshaker at 37 °C, 120 rpm; then, the suspension was centrifuged, and the supernatant was collected to conduct a spectrophotometric quantification of the Nisin released. Spectrophotometric measures were performed using a Nisin calibration curve in a concentration range of 0.05–0.25 mg/mL of Nisin in SBF. After quantification, a new amount of SBF was put in contact with the just-soaked solid, and so on until arriving to the total release of Nisin.

Experiments regarding Nisin stability in SBF were performed to confirm the presence of Nisin after a long period of soaking in SBF, using a reference solution. The time intervals tested were the ones considered for release tests, and a UV-Vis quantification of Nisin confirmed its stability.

2.5. Physical-Chemical Characterization of Powders

2.5.1. Scanning Electron Microscopy (SEM)

The morphology of the unaltered powdery samples, of the loaded powdery samples and of samples after soaking in SBF was examined by SEM-FEG using a SEM Nova NanoSEM 450 (FEI Company, Milan, Italy) microscope operating at 15 kV.

2.5.2. Textural Properties

To evaluate the loading behavior of LPMSs, the surface areas were determined by N_2 adsorption/desorption isotherms carried out at T~77 K using ChemiSorb 2750—Micromeritics (Alfatest S.r.l., Rome, Italy). Adsorption data were processed by the standard Brunauer, Emmet and Teller (BET) method [25] to determine the specific surface area (SSA_{BET}).

The total pore area and the intrusion volume were determined with a mercury porosimeter, using AutoPore IV 9500 (Micrometrics Instrument Corporation, Alfatest S.r.l., Rome, Italy) operating at mercury filling pressure of 1.51 psi.

The pore size can be determined from the pressure value of the liquid through the Washburn equation (Equation (1)), which describes its capillary flow within them.

$$L = \sqrt{\frac{\gamma r t \cos \theta}{2\eta}} \tag{1}$$

where *L* is the penetration length, γ is the surface tension, *r* is the pore radius, θ is the contact angle between the penetrating liquid and pore walls, *t* is the penetration time and η is the dynamic viscosity.

2.5.3. UV-VIS Spectroscopy

To evaluate the amount of Nisin loaded inside the structures and the amount released after soaking with SBF, UV-VIS spectra were acquired. UV-visible spectra were recorded using a JASKO V-570 UV/Vis/NIR (JASCO Europe S.r.l., Cremella, Italy) (spectrophotometer at 298 K in the 190–400 nm spectral range employing quartz cells (1 cm optical path). Nisin quantification was performed at 277 nm.

2.5.4. Elemental Analysis (EA)

EA was performed to confirm data collected with UV-VIS spectra, evaluate the amount of Nisin loaded inside the structures and evaluate its stability, using Thermo Scientific[™] FLASH 2000 CHNS Anal (Thermo Fischer Scientific Inc., Milan, Italy).

A process blank was prepared and analyzed for all samples, and the results show this taken into consideration.

2.5.5. Thermogravimetric Analysis (TG-DTA)

To confirm the presence of stable Nisin onto the structures, TG analyses were performed using a Seiko SSC 5200 in a temperature range between 25 °C and 1000 °C with a heating rate of 1 °C/min.

2.5.6. Confocal Laser Scanning Microscopy (CLSM)

A confocal microscope was used to evaluate the presence of Nisin on the surface of powdery samples loaded with Nisin. Nisin fluorescence was obtained using an exciting wavelength of 405 nm and registering the emission in the range 470–580 nm, using Leica TCS SP8 (Leica Biosystems, Milan, Italy).

3. Results and Discussions

3.1. LPMSs' Morphology Characterization with SEM

To choose the correct time of reaction and the quantity of adjuvant, SEM-FEG characterization of samples was performed.

In this work, we started to study the product of the reaction by fixing the surfactant, and using the classical P123[®] to synthesize MS [26,27]. In Figure 2, the samples differ in terms of the presence or not of the adjuvant and its amount: in LPMS_1_TMB_18h, the quantity of adjuvant is twice with respect to LPMS_2_TMB_18h, and the difference in the aperture of the structure is noticeable; in LPMS_1_18h and LPMS_2_18h, adjuvant is not present, and the structures are more compact. For these reasons, the presence of an adjuvant was considered necessary, and a ratio by mass 1:3.85 TMB:TEOS was fixed.

Then, maintaining the same ratio by mass of TEOS:surfactant at 1.7:1 and TEOS:TMB at 3.85:1 of the synthesis LPMS_1_TMB_18h, and varying only the time of reaction, we tried to reduce it. It is possible to notice from Figure 3, starting from 2 h and arriving up to 8 h, that the only result was that the surface became more and more non-homogeneous, but the best time remains at 18 h.







SEM-FEG images of samples (a) LPMS_1_TMB_18h, (b) LPMS_2_TMB_18h, Figure 2. (c) LPMS_1_18h and (d) LPMS_2_18h.



Figure 3. SEM-FEG images of samples (a) LPMS_1_2h, (b) LPMS_1_4h, (c) LPMS_1_6h and (**d**) LPMS_1_8h.

It is possible to notice from Figures 2 and 3 that the increasing time brings a better aggregation of the silica nanoparticles and that, at 2 h, they are abundantly present compared to at 18 h, when more sintered structures are present.

After thatwe studied if it was possible to obtain better structures by fixing the time at 8 h, and modifying the ratio by mass TEOS:surfactant from 1:1.0 to 1:2.0.

It is possible to see from Figure 4 that an increase in the quantity of surfactant causes an increase in pores' dimensions, which was the intended purpose. For this reason, the ratio by mass of TEOS:surfactant was fixed to 1:2.



(a)



(c)

Figure 4. SEM-FEG images of samples (a) LPMS_3_8h ratio by mass 1:1, (b) LPMS_4_8h ratio by mass 1:1.4 and (c) LPMS_5_8h ratio by mass 1:2. SEM images report the cavity dimensions measured with specific SEM-FEG software tool.

It is clear that 18 h of MW treatment seems to be better to obtain the desired structure, but for studying reasons, we decide to also perform studies on samples obtained with 8 h thermal treatment.

At this point, a new surfactant was studied. Pluronic[®] F127 was considered, thanks to its polyethyleneoxy chain that is five times longer with respect to P123 [28].

Taking into account the previous considerations, a new synthesis was identified: LPMS_7_TMB_18h in which the ratio by mass of TEOS:surfactant was fixed at 1:2 and the ratio by mass of TEOS:TMB was fixed to 3.85:1 with the time of reaction at 18 h.

In Figure 5, is possible to evaluate the difference between LPMS_7_TMB_18h and an equivalent synthesis, LPMS_6_TMB_18h, in which the only difference stays in the surfactant used, which in the second case was P123.



Figure 5. SEM-FEG images of (**a**) LPMS_7_TMB_18h and (**b**) LPMS_6_TMB_18h at different magnifications. The difference between samples stays in surfactant: LPMS_7_TMB_18h is synthesized using F127 and LPMS_6_TMB_18h using P123.

With F127, a great enhancement in the morphology of the structure was obtained: silica nanoparticles were well-sintered and a more open structure and bigger mesopores were obtained. For these reasons, the second surfactant, F127, was the right candidate for our purposes and was fixed as the appropriate surfactant for the next steps.

Additionally, with F127, reactions at 8 h and with different ratios by mass were studied, as reported in Figure 6.

Even with F127, if the ratio by mass between TEOS and the surfactant was changed, a more opened structure was obtained. Additionally, in this case, the ratio of 1:2 was the best.

At this time, as a preliminary analysis, an estimation of pores' dimension [29] and a correlation between their dimensions and the quantity of surfactant was performed, considering the reaction conducted at 8 h with ratios by mass of 1:2.0, 1:1.7, 1:1.4 and 1:1.0. Both surfactants were studied, and the obtained results are reported in Table 2.

Table 2. Pores' dimensions obtained for samples.

	Pores Dimensions ¹ (nm)		
m TEOS:m Surfactant	Pluronic [®] F172	Pluronic [®] P123	
1:2.0	89.7	76.8	
1:1.7	64.2	55.1	
1:1.4	61.3	43.6	
1:1.0	43.5	37.1	

¹ Pores' dimensions calculated as the average of 30 measures collected with the length tool of SEM-FEG software.



Figure 6. SEM-FEG images of samples (**a**) LPMS_8_TMB, (**b**) LPMS_9TMB, (**c**) LPMS_10_TMB and (**d**) LPMS_11_TMB. Ratios of TEOS:surfactant are respectively (**a**) 1:2, (**b**) 1:1.7, (**c**) 1:1.4 and (**d**) 1:1.0.

From the estimation, a linear relationship (Figure 7) between pores' dimensions and the amount of surfactant used in the synthesis, i.e., between pores' dimensions and the ratio by mass, was observed. Additionally, thanks to the bigger dimensions of F127 in terms of the carbon chain, larger pores were obtained with this surfactant [30].



Figure 7. Graph of linear correlation between pores' dimensions (calculated with the length tool of SEM-FEM software ESPRIT 2.1) and ratio of TEOS:surfactant used for the syntheses.

For these reasons, to achieve our purposes, the optimal ratio by mass was 1:2.0, and F127 was the appropriate surfactant.

This determination was performed with exploratory purposes, and samples selected for the following studies were completely and properly characterized (see Section 2: Textural Properties).

To summarize all our findings: the presence of an adjuvant helps to obtain bigger pores, so TMB was necessary; the best structures in terms of compactness were obtained at a higher reaction time; therefore, samples obtained at 8 h and 18 h were considered in the next steps; the best surfactant is the biggest one; consequently, F127 was chosen; at a higher ratio by mass, bigger pores were obtained, and a ratio of 1:2 of TEOS:surfactant was fixed.

Taking into account all these considerations, the samples studied in the next steps will be LPMS_8_TMB_8h and LPMS_7_TMB_18h.

SEM-FEG characterization (Figure 8) was also performed for structures used as a reference in loading and release tests. Reference structures considered were MS and silica with no mesopores, only containing micropores (without mesoporous silica, WMS).



Figure 8. SEM-FEG images of samples (a) MS and (b) WMS at different magnifications.

It is possible to see, that both structures look compact if compared with the same magnification of LPMS_8_TMB_8h or LPMS_7_TMB_18h, respectively, reported in Figures 4 and 5.

3.2. Textural Properties

 N_2 adsorption/desorption and mercury impregnation measurements were performed to evaluate and compare the textural properties of samples, determining the following: specific surface area (SSA_{BET}), total pore area (A_p) and total intrusion volume (V_p). The first parameter was determined with N₂ adsorption/desorption method as a mean of three different and independent measurements, and the others with mercury impregnation. In Table 3, the textural parameters of samples are reported. Adsorption/desorption isotherms based on which the surface area values were obtained are presented in Figure 9. As it is possible to see from Figure 9, a different behavior between MS and LPMSs is evident: from the dashed lines, the intrusion in pores of big dimensions for LPMSs is noticeable, which is not detectable for MS and WMS.

Table 3. SSA_{BET}, A_P and V_p of samples subjected to loading and release tests.

Sample	SSA _{BET} (m ² /g)	$A_P (m^2/g)$	V _p (mL/g)
LPMS_8_TMB_8h	309 ± 15	421	2.36
LPMS_7_TMB_18h	330 ± 17	499	3.57
MS	323 ± 16	289	1.49
WMS	404 ± 21	50	0.78



Figure 9. Adsorption/desorption isotherms based on which the surface area values were obtained. From cumulative intrusion (dashed line), it is possible to notice a different behavior between MS and LPMS.

 SSA_{BET} was not significantly different between samples considered. WMS shows the highest value, due to the presence of micropores that significantly enhance this value. LPMS_8_TMB_8h and LPMS_7_TMB_18h show a value of SSA_{BET} that is consistent with the values obtained for classical MS [31]. This behavior can be justified by also considering the other values (A_p and V_p), which are significantly higher for LPMSs with respect to the other structures [32].

 A_p has the lowest values for WMS, which in line with the results considering that the sample only has micropores and the porosimeter cannot measure their pore area; MS, SSA_{BET} and A_p are comparable, instead of LPMSs that show an SSA_{BET} lower than the A_p . It can be explained considering that SSA_{BET} was calculated using N₂ adsorption/desorption and that Ap uses Hg; the latter can fill big pores, instead of N₂, which can only create a layer on the surface of them, so it turns out that A_p can have higher values if compared to SSA_{BET} [33].

The mercury impregnation method can determine pores only in the range of $3.5-300 \ \mu\text{m}$. Figure 10 reports results obtained with the mercury porosimeter, and the classification of pores due to dimensions according to the IUPAC scheme [34] and a new scheme proposed by T. J. Mays, et al. [35]. According to particle dimensions, supermicropores can be considered interparticle pores. Pores under 10 μ m can be classified, in order of dimensions, as follows: inter-nanopores (1–10 nm), super-nanopores (10–100 nm) and sub-micropores (100–1000 nm). Samples studied in this work present different characteristics in terms of pores, and the type and number of pores present in their structure are summarized in Table 4.



Figure 10. On the top: results obtained with the mercury porosimeter, and a graph of the distribution of pore volume as a function of pore size. In the bottom: pore classification due to dimension according to the IUPAC scheme and a new scheme proposed by T. J. Mays et al. [35].

Table 4. Type and number of pores of samples at a certain range of dimensions.

	3–10 nm	10–30 nm	500–600 nm	10–200 μm
Sample	Inter-Pore	Super-Nanopore	Sub-Micropore	Super-Micropore
LPMS_8_TMB_8h	++++	++	-	++++
LPMS_7_TMB_18h	+++++	+++	+++	++++
MS	+++	-	-	++++
WMS	+	-	-	++

The number of "+" schematically indicates the number of pores at a certain dimension.

3.3. Nisin Loading Tests

The efficiency of the loading of a molecule into a structure can be calculated in different ways, using the following: loading efficiency percentage (LE%), loading percentage (Loading%) or loading capacity percentage (LC%).

The loading efficiency percentage (Equation (2)) considers the only amount of Nisin loaded inside the structure as a function of the initial quantity used for loading [36]:

$$LE\% = \frac{Amount \ of \ Nisin \ loaded \ (mg)}{Initial \ amount \ of \ Nisin \ (mg)} \cdot 100$$
(2)

The initial amount of Nisin was determined directly using a spectrophotometric quantification of the concentration of the loading solution; then, the amount of Nisin

loaded can be determined as the difference between the initial concentration and the concentration after loading, which is always determined by spectrophotometric measure.

The loading percentage (Equation (3)) considers the amount of Nisin loaded as a function of the total weight of the loaded structure [37]:

$$Loading\% = \frac{Amount \ of \ Nisin \ loaded \ (mg)}{Weight \ of \ loaded \ structure \ (silica + Nisin) \ (mg)} \cdot 100$$
(3)

Loading% can be also calculated, to compare results, using the EA results as follows (Equation (4)):

$$LE\% = \frac{\% C determined with EA}{Theorethical \%C} \cdot 100$$
(4)

Finally, the loading capacity percentage was calculated as a function of the amount of Nisin per milligrams of silica (Equation (5)) [38,39]:

$$LC\% = \frac{Amount \ of \ Nisin \ loaded \ (mg)}{Silica \ amount \ (mg)} \cdot 100 \tag{5}$$

EA was performed on solids collected after loading and dried overnight. In Table 5, the EA and samples are reported and were labeled as "sample_name_x" in which x indicates the concentration of Nisin (in mg/mL) in the loading solution.

Sample	%C	%H	%N	%S
LPMS_8_TMB_8h_0.5	0.78	0.36	0.25	0.00
LPMS_8_TMB_8h_1	0.80	0.31	0.26	0.00
LPMS_8_TMB_8h_1.2	1.88	0.58	0.67	0.08
LPMS_8_TMB_8h_1.35	1.96	0.50	0.58	0.00
LPMS_8_TMB_8h_5	7.21	1.30	2.17	0.00
LPMS_8_TMB_8h_10	10.27	1.99	3.36	0.50
LPMS_8_TMB_8h_20	13.05	1.85	4.24	0.64
LPMS_7_TMB_18h_0.5	0.58	0.23	0.22	0.00
LPMS_7_TMB_18h_1	0.97	0.30	0.39	0.00
LPMS_7_TMB_18h_1.2	1.49	0.36	0.52	0.00
LPMS_7_TMB_18h_1.35	1.83	0.48	0.55	0.08
LPMS_7_TMB_18h_5	6.56	1.09	2.20	0.32
LPMS_7_TMB_18h_10	10.99	1.35	3.79	0.00
LPMS_7_TMB_18h_20	11.70	1.60	4.02	0.20
MS_0.5	0.51	0.08	0.15	0.00
MS_1	0.73	0.10	0.22	0.00
MS_1.2	0.92	0.13	0.28	0.00
MS_1.35	1.01	0.15	0.30	0.00
MS_5	4.12	0.83	1.30	0.06
MS_10	6.77	0.89	2.21	0.05
WMS_0.5	0.29	0.32	0.11	0.00
WMS_1	0.39	0.69	0.15	0.00
WMS_1.2	0.54	0.00	0.20	0.00
WMS_1.35	0.46	0.08	0.00	0.00
WMS_5	1.06	0.61	0.38	0.00
WMS_10	7.85	1.14	2.77	0.24
WMS_20	10.09	1.70	3.41	0.43

Table 5. Results of EA performed on loaded structures dried overnight at 70 °C.

EA results were used to calculate loading% and to evaluate the stability of Nisin loaded into the structures. As it is possible to see from Table 4 that the results are in accordance with the concentration of the loading solution: the higher the concentration, the higher the percentage of each element in the structures.

To evaluate the presence of Nisin on the surface of the structures, %N vs. %C obtained with EA were plotted for all samples (Figure 11), and the slope of linear regression obtained was compared to the ratio N/N calculated for pure Nisin. Considering the Nisin molecular formula ($C_{143}H_{230}N_{42}O_{37}S_7$), a N/N c of 0.343 is obtained, which is perfectly in line with the result if compared to the 0.333 obtained with experimental linear regression. For this reason, it can be confirmed that the loaded Nisin is still present, but to assert the presence of non-degraded Nisin and also confirm its presence in the structures after various weeks, a UV-Vis determination is necessary. This aspect will be treated in Section 4: Results and Discussion.



Figure 11. Linear regression was obtained by plotting %N depending on the %C obtained from EA. In the graph, all studied and loaded samples are reported.

Comparing LE%, LC% and loading% reported in Table 6 and in Figure 12, it could be noticed that the LE% for LPMS_8_TMB_8h and LPMS_7_TMB_18h does not vary significantly at the different loading concentrations and always stays in a range between 50 and 90%, instead of MS, which shows a LE% in the range 20–30%, which is significantly lower than LPMSs; WMS has a LE% that varies exponentially, synonymous with a process under precipitation control. The same results were obtained for Loading%. These effects are caused by the dimensions of pores: for LPMSs, Nisin can fill very large cavities, and the trapped amount is up to 3/4 times higher with respect to classical structures; in MS and WMS, Nisin can stay only on the surface, and the Nisin amount detected is the Nisin precipitated on the surface. This way of loading will bring very fast and not controlled releases, if compared to LPMSs. LC% has, for all samples, an exponential behavior because the more Nisin in the solution, there is more quantity that can be trapped or that can recover the surface.



Figure 12. LE%, loading% and LC% of all samples reported in Table 5 are graphed in a bar graph to better understand and compare data collected for LPMSs, MS and WMS.

Sample	LE%	LC%	Loading%	Loading% Calculated with EA
LPMS_8_TMB_8h_0.5	75.8	1.9	1.8	1.7
LPMS_8_TMB_8h_1	81.0	3.1	3.0	1.7
LPMS_8_TMB_8h_1.2	76.9	3.6	3.5	3.8
LPMS_8_TMB_8h_1.35	70.7	3.8	3.7	4.0
LPMS_8_TMB_8h_5	74.5	16.1	13.8	14.2
LPMS_8_TMB_8h_10	72.1	29.0	26.6	20.2
LPMS_8_TMB_8h_20	80.5	60.4	43.0	25.6
LPMS_7_TMB_18h_0.5	53.6	1.2	1.2	1.3
LPMS_7_TMB_18h_1	70.2	2.5	2.5	2.0
LPMS_7_TMB_18h_1.2	78.2	3.5	3.4	3.0
LPMS_7_TMB_18h_1.35	79.7	4.3	4.1	3.7
LPMS_7_TMB_18h_5	93.1	22.1	18.1	12.9
LPMS_7_TMB_18h_10	72.6	31.8	24.1	21.6
LPMS_7_TMB_18h_20	83.5	71.4	41.7	23.0
MS_0.5	25.3	0.9	0.9	1.0
MS_1	22.2	1.2	1.2	1.5
MS_1.2	21.0	1.6	1.5	1.8
MS_1.35	26.2	2.6	2.5	2.0
MS_5	21.8	7.9	7.3	8.1
MS_10	30.7	21.6	17.8	13.3
MS_20	29.0	45.0	27.6	26.8
WMS_0.5	0.0	0.0	0.0	0.6
WMS_1	0.0	0.0	0.0	0.8
WMS_1.2	0.0	0.0	0.0	1.1
WMS_1.35	0.0	0.0	0.0	0.9
WMS_5	3.8	0.9	0.9	2.1
WMS_10	38.9	17.6	15.0	15.4
WMS_20	65.3	55.9	35.8	19.7

Table 6. LE%, LC%, loading% and loading% calculated with EA of all samples studied.

The Loading% values calculated with EA results are consistent with the ones calculated spectrophotometrically.

TGA-DTA was performed on structures with a comparable LC%, to obtain a decomposition of Nisin in the same mass range, i.e., LPMS_8_TMB_8h_1.35, LPMS_7_TMB_18h_1.35, MS_1.35 and WMS_5.

TGA (Figure 13) confirmed the results obtained with the previous analysis, and the loss in mass obtained with thermal analysis is comparable to the amount of Nisin established with EA and UV-VIS determination (Table 7). To determine the loss in mass of loaded structures, unprocessed samples were also analyzed as a blank reference. From the TG derivative graph (DTG) (Figure 14), a delay in decomposition, with respect to pure Nisin, was observed for all samples, probably caused by the interaction between Nisin and the silica surface. The same derivative shapes of a sample of pure Nisin were obtained, confirming the presence and stability of Nisin loaded onto the structures. In the derivative graph, the first peak at 300 °C is attributable to the pyrolysis of Nisin (*), and the second one (**) at about 480 °C is attributable to the decomposition of the peptide structure [40].

BET was determined for all loaded samples to evaluate the behavior of LPMS and MS. From SSA_{BET} values plotted as a function of LC% (Figure 15), it is possible to see that LPMSs show a lower decrease in SSA if compared to MS; considering the difference in LE% between samples, this behavior could be explained considering first the filling of pores and then, at high concentration, the covering of the surface for LPMSs that permit the slowest decrease of SSA_{BET}, instead of MS, which undergoes a pore blocking [41,42], which is well-known for mesoporous materials. Additionally, superficial analysis confirms the different behavior between WMS and other samples.



Figure 13. TG graph of loaded samples (full lines) and unprocessed samples (dashed lines). From the differences between curves, it is possible to calculate the loss in mass related to the Nisin content.

Table 7. Total amount of Nisin (calculated as LC%) inside structures determined with different analyses.

	Nisin Content—Different Determination Techniques		
Sample	UV-Vis	TG	
LPMS_8_TMB_8h_1.35	3.8 mg/100 mg	4.2 mg/100 mg	
LPMS_7_TMB_18h_1.35	4.3 mg/100 mg	4.7 mg/100 mg	
MS_1.35	2.6 mg/100 mg	2.8 mg/100 mg	
WMS_5	0.9 mg/100 mg	1.2 mg/100 mg	



Figure 14. DTG, derivative graph obtained from TG curves. *, peak relative to pyrolisis of Nisin; **, peak relative to the decomposition of Nisin.



Figure 15. SSA_{BET} determined on unadulterated powders and on loaded powders, plotted as a function of LC%. Data are reported as a mean of three different measures performed on three different amounts of sample.

3.4. Nisin Release Tests

To evaluate Nisin stability, Nisin release tests were performed on loaded structures a few weeks after loadings. The Nisin content obtained spectrophotometrically and with EA is comparable, so can be asserted that Nisin is present and stable.

Nisin release tests were performed for structures with a comparable Loading%, i.e., LPMS_8_TMB_8h_5, LPMS_7_TMB_18h_5, MS_10 and WMS_10, which all have a Loading% of about 15%.

The amount of Nisin released was determined as % of release (Equation (5)):

% release =
$$\frac{Cumulative amount of Nisin released at a certain time}{Total Nisin content} \cdot 100$$
 (6)

Starting from samples with the same Nisin content, a four time longer release and controlled mechanism of release can be achieved for LPMSs (Figure 16). MS exhibits a shorter release, and even shorter for WMS, of about 1 day and 1 h, respectively, in comparison to 4 days of LPMSs. LPMSs' releases are definitely longer if compared with the time of the release of MS and previous studies [43]: LPMSs show releases that last 96 h, instead of MS, which shows a four time shorter release of about 24 h (results in line with previous studies).



Figure 16. %Release determined with UV-Vis analysis plotted as a function of time.

Another important aspect is the mechanical resistance that LPMS_7_TMB_18h shows after being kept in contact with SBF for a lot of hours. In Figure 17, we report the SEM-FEG images of unaltered structures, loaded structures and structures after soaking in SBF.

After release, LPMS_7_TMB_18h maintains its structure, synonymous with mechanical resistance; LPMS_8_TMB_8h does not have the same mechanical resistance, synonymous with the fact that a longer thermal treatment is necessary to obtain structures that can resist over time when used as support for drug release. For MS and WMS, after a release of 24 h or 1 h, respectively, the structures are maintained.

CLSM was used to visibly evaluate Nisin loading. In Figure 18, microscope images obtained for loaded samples and samples after release are reported.



Figure 17. SEM-FEG images acquired on samples (**a**) LPMS_7_TMB_18h_5, (**b**) LPMS_8_TMB_8h_5, (**c**) MS_10 and (**d**) WMS_10, studied unaltered, after loading and after release tests in SBF.



Figure 18. Confocal laser scanning microscopy images acquired on samples (**a**) LPMS_7_TMB_18h_5, (**b**) LPMS_8_TMB_8h_5, (**c**) MS_10 and (**d**) WMS_10 studied when loaded and after release in SBF.

As it is possible to see from a comparison between the first and the second row in Figure 18, the confocal microscope images confirm the same patterns observed at SEM-FEG: the structure of LPMS_8_TMB_18h is also maintained after loading and the pores are visibly filled with Nisin, LPMS_7_TMB_8h after loading has a more compact structure due to the filling of superficial cavities and MS and WMS pass from a smooth surface to a non-homogeneous surface due to Nisin precipitation on the surface of the microparticles.

The hypothesis of an in-pore drug loading for LPMSs and an external deposition of Nisin for MS and WMS was confirmed.

In fact, loaded structures of MS and WMS show a change in the superficial aspect, indicating that Nisin precipitates on the surface, and for LPMSs, it is noticeable for the filling of pores.

In addition, complete releases can be demonstrated. As it is possible to see from images, the fluorescence of samples is highly quenched, synonymous with an almost complete release.

4. Conclusions, Limitations and Prospects

In light of the results obtained, it can be concluded that a new synthesis pathway to obtain LPMSs has been drawn, and this study, concerning a better surfactant and reaction time, shows that a different methodology with respect to the old one has to be adopted, in terms of the surfactant, time, temperature and conditions of reaction.

In loading and release tests, LPMSs show improved characteristics with respect to the old structures, in terms of LE%, LC%, controlled and longer release and mechanical resistance in physiological environment.

In conclusion, LPMSs (in particular, LPMS_7_TMB_18h) are good candidates for reaching high loading and controlled drug release of big pharmaceutical molecules, thanks to the structured pore system and mechanical resistance. Their utilization in studying the mobility of large organic molecules could be considered in a confined state [44]. However, the weak point of synthesized structures could be the superficial pores' blocking act by substances that can be found in vivo, such as cells.

Author Contributions: Conceptualization, G.M. and D.C.; methodology, G.M.; investigation, D.C.; resources, G.M. and E.F.; data curation, D.C.; writing—original draft preparation, D.C.; writing—review and editing, D.C., G.M. and E.F.; supervision, G.M. and E.F.; project administration, G.M. and E.F.; funding acquisition, G.M. All authors have read and agreed to the published version of the manuscript.

Funding: This research received no external funding.

Institutional Review Board Statement: Not applicable.

Informed Consent Statement: Not applicable.

Data Availability Statement: Additional data that support the findings of this study are available from the corresponding author.

Acknowledgments: The authors would like to thank Jonathan Vinet of the Centro Interdipartimentale Grandi Strumenti of University of Modena and Reggio Emilia for the helpful assistance for aquiring Confocal laser scanning microscopy images.

Conflicts of Interest: The authors declare no conflict of interest.

References

- Bechinger, B.; Gorr, S.-U. Antimicrobial Peptides: Mechanisms of Action and Resistance. J. Dent. Res. 2017, 96, 254–260. [CrossRef] [PubMed]
- Lázár, V.; Martins, A.; Spohn, R.; Daruka, L.; Grézal, G.; Fekete, G.; Számel, M.; Jangir, P.; Kintses, B.; Csörgő, B.; et al. Antibioticresistant bacteria show widespread collateral sensitivity to antimicrobial peptides. *Nat. Microbiol.* 2018, *3*, 718–731. [CrossRef] [PubMed]
- Faya, M.; Kalhapure, R.S.; Kumalo, H.M.; Waddad, A.Y.; Omolo, C.; Govender, T. Conjugates and nano-delivery of antimicrobial peptides for enhancing therapeutic activity. J. Drug. Deliv. Sci. Technol. 2018, 44, 153–171. [CrossRef]
- 4. Tornesello, A.L.; Borrelli, A.; Buonaguro, L.; Buonaguro, F.M.; Tornesello, M.L. Antimicrobial Peptides as Anticancer Agents: Functional Properties and Biological Activities. *Molecules* **2020**, *25*, 2850. [CrossRef] [PubMed]
- Wan, L.; Chen, Z.; Deng, Y.; Liao, T.; Kuang, Y.; Liu, J.; Duan, J.; Xu, Z.; Jiang, B.; Li, C. A novel intratumoral pH/redoxdual-responsive nanoplatform for cancer MR imaging and therapy. *J. Colloid. Interface Sci.* 2020, 573, 263–277. [CrossRef] [PubMed]
- 6. Mendez-Samperio, P. Peptidomimetics as a new generation of antimicrobial agents: Current progress. *Infect. Drug. Resist.* 2014, 7, 229–237. [CrossRef]

- Domhan, C.; Uhl, P.; Meinhardt, A.; Zimmermann, S.; Kleist, C.; Lindner, T.; Leotta, K.; Mier, W.; Wink, M. A novel tool against multiresistant bacterial pathogens: Lipopeptide modification of the natural antimicrobial peptide ranalexin for enhanced antimicrobial activity and improved pharmacokinetics. *Int. J. Antimicrob. Agents* 2018, 52, 52–62. [CrossRef]
- Wang, C.; Liu, X.; Chen, S.; Hu, F.; Sun, J.; Yuan, H. Facile preparation of phospholipid–amorphous calcium carbonate hybrid nanoparticles: Toward controllable burst drug release and enhanced tumor penetration. *Chem. Commun.* 2018, 54, 13080–13083. [CrossRef]
- Reuther, J.F.; Dees, J.L.; Kolesnichenko, I.V.; Hernandez, E.T.; Ukraintsev, D.V.; Guduru, R.; Whiteley, M.; Anslyn, E.V. Dynamic covalent chemistry enables formation of antimicrobial peptide quaternary assemblies in a completely abiotic manner. *Nat. Chem.* 2018, 10, 45–50. [CrossRef]
- Braun, K.; Pochert, A.; Gerber, M.; Raber, H.F.; Lindén, M. Influence of mesopore size and peptide aggregation on the adsorption and release of a model antimicrobial peptide onto/from mesoporous silica nanoparticles in vitro. *Mol. Syst. Des. Eng.* 2017, 2, 393–400. [CrossRef]
- 11. Ma, Z.; Bai, J.; Wang, Y.; Jiang, X. Impact of Shape and Pore Size of Mesoporous Silica Nanoparticles on Serum Protein Adsorption and RBCs Hemolysis. *ACS Appl. Mater. Interfaces* **2014**, *6*, 2431–2438. [CrossRef] [PubMed]
- Nicolini, V.; Malavasi, G.; Lusvardi, G.; Zambon, A.; Benedetti, F.; Cerrato, G.; Valeri, S.; Luches, P. Mesoporous bioactive glasses doped with cerium: Investigation over enzymatic-like mimetic activities and bioactivity. *Ceram. Int.* 2019, 45, 20910–20920. [CrossRef]
- 13. Wang, C.; Hong, T.; Cui, P.; Wang, J.; Xia, J. Antimicrobial peptides towards clinical application: Delivery and formulation. *Adv. Drug. Deliv. Rev.* **2021**, 175, 113818. [CrossRef]
- 14. Zhoua, Y.; Quana, G.; Wub, Q.; Zhangc, X.; Niua, B.; Wua, B.; Huanga, Y.; Pana, X.; Wuad, C. Mesoporous silica nanoparticles for drug and gene delivery. *Acta Pharm. Sin. B* 2018, *8*, 165–177. [CrossRef]
- 15. Gao, F.; Botella, P.; Corma, A.; Blesa, J.; Dong, L. Monodispersed Mesoporous Silica Nanoparticles with Very Large Pores for Enhanced Adsorption and Release of DNA. *J. Phys. Chem. B* **2009**, *113*, 1796–1804. [CrossRef] [PubMed]
- 16. Zhang, X.; Zeng, D.; Li, N.; Jiang, X.; Liu, C.; Li, Y. Large-pore mesoporous Ca–Si-based bioceramics with high in vitro bioactivity and protein adsorption capability for bone tissue regeneration. *J. Mater. Chem. B* **2016**, *4*, 3916–3924. [CrossRef] [PubMed]
- 17. Moghaddam, S.P.H.; Yazdimamaghani, M.; Ghandehari, H. Glutathione-sensitive hollow mesoporous silica nanoparticles for controlled drug delivery. J. Control Release 2018, 282, 62–75. [CrossRef]
- 18. Gisbert-Garzarán, M.; Vallet-Regí, M. Redox-Responsive Mesoporous Silica Nanoparticles for Cancer Treatment: Recent Updates. *Nanomaterials* **2021**, *11*, 2222. [CrossRef]
- 19. Bansal, A.; Celeste Simon, M. Glutathione metabolism in cancer progression and treatment resistance. *J. Cell. Biol.* **2018**, 217, 2291–2298. [CrossRef]
- 20. Han, Y.; Ying, J.Y. Generalized Fluorocarbon-Surfactant-Mediated Synthesis of Nanoparticles with Various Mesoporous Structures. *Angew. Chem. Int. Ed.* **2005**, *44*, 288–292. [CrossRef]
- Shin, J.; Gwak, J.; Kamarajan, P.; Fenno, J.; Rickard, A.; Kapila, Y. Biomedical applications of nisin. J. Appl. Microbiol. 2016, 120, 1449–1465. [CrossRef] [PubMed]
- 22. Flynn, J.; Mallen, S.; Durack, E.; O'Connor, P.M.; Hudson, S.P. Mesoporous matrices for the delivery of the broad spectrum bacteriocin, nisin A. J. Colloid. Interface Sci. 2019, 537, 396–406. [CrossRef]
- Sobrino-López, A.; Martín-Belloso, O. Use of nisin and other bacteriocins for preservation of dairy products. *Int. Dairy*, J. 2008, 18, 329–343. [CrossRef]
- 24. Brum, L.F.W.; dos Santos, C.; Santos, J.H.Z.; Brandelli, A. Structured silica materials as innovative delivery systems for the bacteriocin nisin. *Food Chem.* 2022, *366*, 130599. [CrossRef]
- 25. Brunauer, S.; Emmett, P.H.; Teller, E. Adsorption of Gases in Multimolecular Layers. J. Am. Chem. Soc. 1938, 60, 309–319. [CrossRef]
- Bharatiya, B.; Ghosh, G.; Bahadur, P.; Mata, J. The Effects of Salts and Ionic Surfactants on the Micellar Structure of Tri-Block Copolymer PEO-PPO-PEO in Aqueous Solution. J. Dispers. Sci. Technol. 2008, 29, 696–701. [CrossRef]
- Poyraz, A.S.; Dag, Ö. Role of Organic and Inorganic Additives on the Assembly of CTAB-P123 and the Morphology of Mesoporous Silica Particles. J. Phys. Chem. C 2009, 113, 18596–18607. [CrossRef]
- 28. Pitto-Barry, A.; Barry, N.P.E. Pluronic®block-copolymers in medicine: From chemical and biological versatility to rationalisation and clinical advances. *Polym. Chem.* 2014, *5*, 3291–3297. [CrossRef]
- Horvat, G.; Pantić, M.; Knez, Ž.; Novak, Z. A Brief Evaluation of Pore Structure Determination for Bioaerogels. *Gels* 2022, *8*, 438. [CrossRef]
- Varini, E.; Sánchez-Salcedo, S.; Malavasi, G.; Lusvardi, G.; Vallet-Regí, M.; Salinas, A.J. Cerium (III) and (IV) containing mesoporous glasses/alginate beads for bone regeneration: Bioactivity, biocompatibility and reactive oxygen species activity. *Mater. Sci. Eng. C* 2019, 105, 109971. [CrossRef]
- Ganguly, A.; Ahmad, T.; Ganguli, A.K. Silica Mesostructures: Control of Pore Size and Surface Area Using a Surfactant-Templated Hydrothermal Process. *Langmuir* 2010, 26, 14901–14908. [CrossRef]
- 32. Brown, S.M.; Lard, E.W. A comparison of nitrogen and mercury pore size distributions of silicas of varying pore volume. *Powder Technol.* **1974**, *9*, 187–190. [CrossRef]

- Lei, Q.; Guo, J.; Noureddine, A.; Wang, A.; Wuttke, S.; Brinker, C.J.; Zhu, W. Sol–Gel-Based Advanced Porous Silica Materials for Biomedical Applications. *Adv. Funct. Mater.* 2020, *30*, 1909539. [CrossRef]
- Sing, K.S.W.; Everett, D.H.; Haul, R.A.W.; Moscou, L.; Pierotti, R.A.; Rouquerol, J.; Siemieniewska, T. Reporting Physisorption Data for Gas/Solid Systems with Special Reference to the Determination of Surface Area and Porosity. *Pure Appl. Chem.* 1984, 57, 603–619. [CrossRef]
- 35. Mays, T. A new classification of pore sizes. *Stud. Surf. Sci. Catal.* 2007, 160, 57–62. [CrossRef]
- Kassem, M.A.; El-Sawy, H.S.; Allah, F.A.; Abdelghany, T.M.; El-Say, K.M. Maximizing the Therapeutic Efficacy of Imatinib Mesylate–Loaded Niosomes on Human Colon Adenocarcinoma Using Box-Behnken Design. J. Pharm. Sci. 2017, 106, 111–122. [CrossRef]
- 37. Ibrahim, A.H.; Smått, J.-H.; Govardhanam, N.P.; Ibrahim, H.M.; Ismael, H.R.; Afouna, M.I.; Samy, A.M.; Rosenholm, J.M. Formulation and optimization of drug-loaded mesoporous silica nanoparticle-based tablets to improve the dissolution rate of the poorly water-soluble drug silymarin. *Eur. J. Pharm. Sci.* **2020**, *142*, 105103. [CrossRef]
- Shen, S.; Wu, Y.; Liu, Y.; Wu, D. High drug-loading nanomedicines: Progress, current status, and prospects. Int. J. Nanomed. 2017, 12, 4085–4109. [CrossRef]
- El-Say, K.M. Maximizing the encapsulation efficiency and the bioavailability of controlled-release cetirizine microspheres using Draper–Lin small composite design. *Drug. Des. Dev. Ther.* 2016, 10, 825–839. [CrossRef]
- 40. Badea, E.; Carşote, C.; Hadîmbu, E.; Şendrea, C.; Lupaş, M.-C. The effect of halloysite nanotubes dispersions on vegetable-tanned leather thermal stability. *Herit. Sci.* **2019**, *7*, 68. [CrossRef]
- Grünberg, B.; Emmler, T.; Gedat, E.; Shenderovich, I.; Findenegg, G.H.; Limbach, H.-H.; Buntkowsky, G. Hydrogen Bonding of Water Confined in Mesoporous Silica MCM-41 and SBA-15 Studied by¹H Solid-State NMR. *Chem. A Eur. J.* 2004, 10, 5689–5696. [CrossRef] [PubMed]
- Petrisor, G.; Ficai, D.; Motelica, L.; Trusca, R.D.; Bîrcă, A.C.; Vasile, B.S.; Voicu, G.; Oprea, O.C.; Semenescu, A.; Ficai, A.; et al. Mesoporous Silica Materials Loaded with Gallic Acid with Antimicrobial Potential. *Nanomaterials* 2022, *12*, 1648. [CrossRef] [PubMed]
- 43. Carrozza, D.; Malavasi, G.; Ferrari, E.; Menziani, M.C. Alginate Beads Containing Cerium-Doped Mesoporous Glass and Curcumin: Delivery and Stabilization of Therapeutics. *Int. J. Mol. Sci.* **2023**, *24*, 880. [CrossRef] [PubMed]
- 44. Shenderovich, I.G. For Whom a Puddle Is the Sea? Adsorption of Organic Guests on Hydrated MCM-41 Silica. *Langmuir* 2020, 36, 11383–11392. [CrossRef] [PubMed]

Disclaimer/Publisher's Note: The statements, opinions and data contained in all publications are solely those of the individual author(s) and contributor(s) and not of MDPI and/or the editor(s). MDPI and/or the editor(s) disclaim responsibility for any injury to people or property resulting from any ideas, methods, instructions or products referred to in the content.